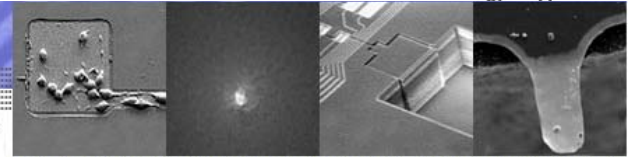




Laboratory of Integrated Bio Medical  
Micro/Nanotechnology & Applications

LIBNA is focused on research in BioMEMS & Bionanotechnology, in the areas of interface between micro, nanoengineering & life sciences



# Interfacing Biology and Engineering at the Micro and Nano Scale

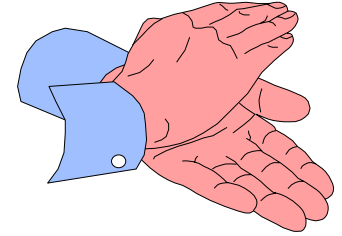
March 8<sup>th</sup>, 2008  
Institute of Biological Engineering  
2008 Annual Conference

***Rashid Bashir***

***Micro and Nanotechnology Laboratory  
Electrical and Computer Engineering & BioEngineering  
University of Illinois, Urbana-Champaign  
<http://libna.micro.uiuc.edu/>***



# Acknowledgements



## Researchers:

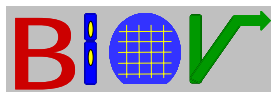
- Prof. Demir Akin
- Dr. JeongMi Moon
- Piyush Bajaj
- Vincent Chan
- Brian Dorvell
- Oguz Elibol
- Yi-Shao Liu
- Kidong Park
- Bobby Reddy
- Shuaib Salamat
- Murali Venkatesan
- Nick Watkins



## Recent Alums

- Prof. J. Jang, Prof. S. Iqbal, Prof. S. W. Lee, Prof. L. Yang,

## **BioVitesse, Inc. Co-Founder**



## Funding Agencies

- National Institute of Health, NIBIB
- NASA Institute on Nano-electronics and Computing (INAC)
- US Department of Agriculture (Center for Food Safety Engineering at Purdue)
- NSF NSEC at OSU
- NIH Nanomedicine NDC

## Faculty Collaborators

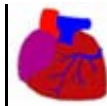
- Prof. A. Alam (ECE, Purdue)
- Prof. D. Bergstrom (Med Chem, Purdue)
- Prof. A. Bhunia (Food Science, Purdue)
- Prof. S. Claire (IU-SOM)
- Prof. P. Guo (Vet Medicine, BME, Univ. of Cincinnati)
- Prof. M. Ladisch (Ag& Bio Engr, Purdue)
- Prof. M. Toner (Harvard Med School)
- Prof. J. P. Robinson (BMS, BME, Purdue)
- Prof. W. Rodriguez (Harvard Med School)



# On Size and Scale ! *Top-Down Fabrication*

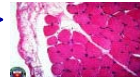
Feature Size

100mm



Organs

10mm



Tissue

1mm



Ants

100μm



Plant and Animal Cells

10μm

Most Bacteria



1μm

100nm

Virus



10nm

Proteins



Helical Turn of DNA

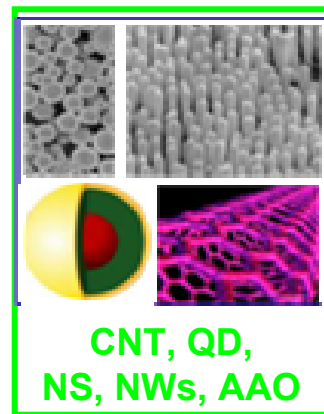
1nm



C-C Bond

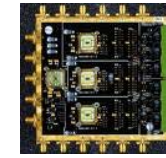
0.1nm

*Bottoms-Up  
Biological*

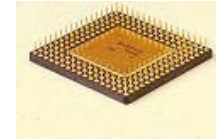


*Bottoms-Up  
Chemical*

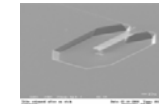
System on  
A board



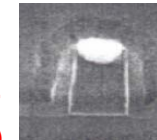
System on  
a chip



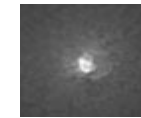
MEMS



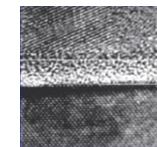
35nm Feat.  
of MOS-T  
(in 2008)



Nano  
pores<sup>-</sup>



Gate  
Insulator

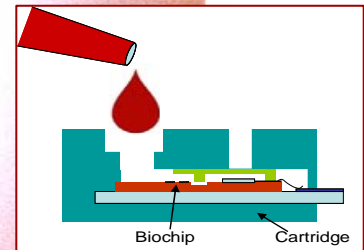
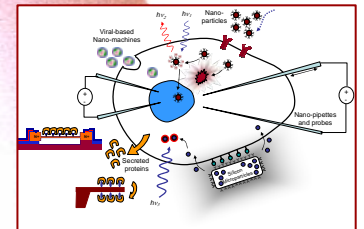
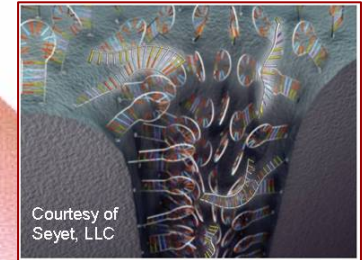
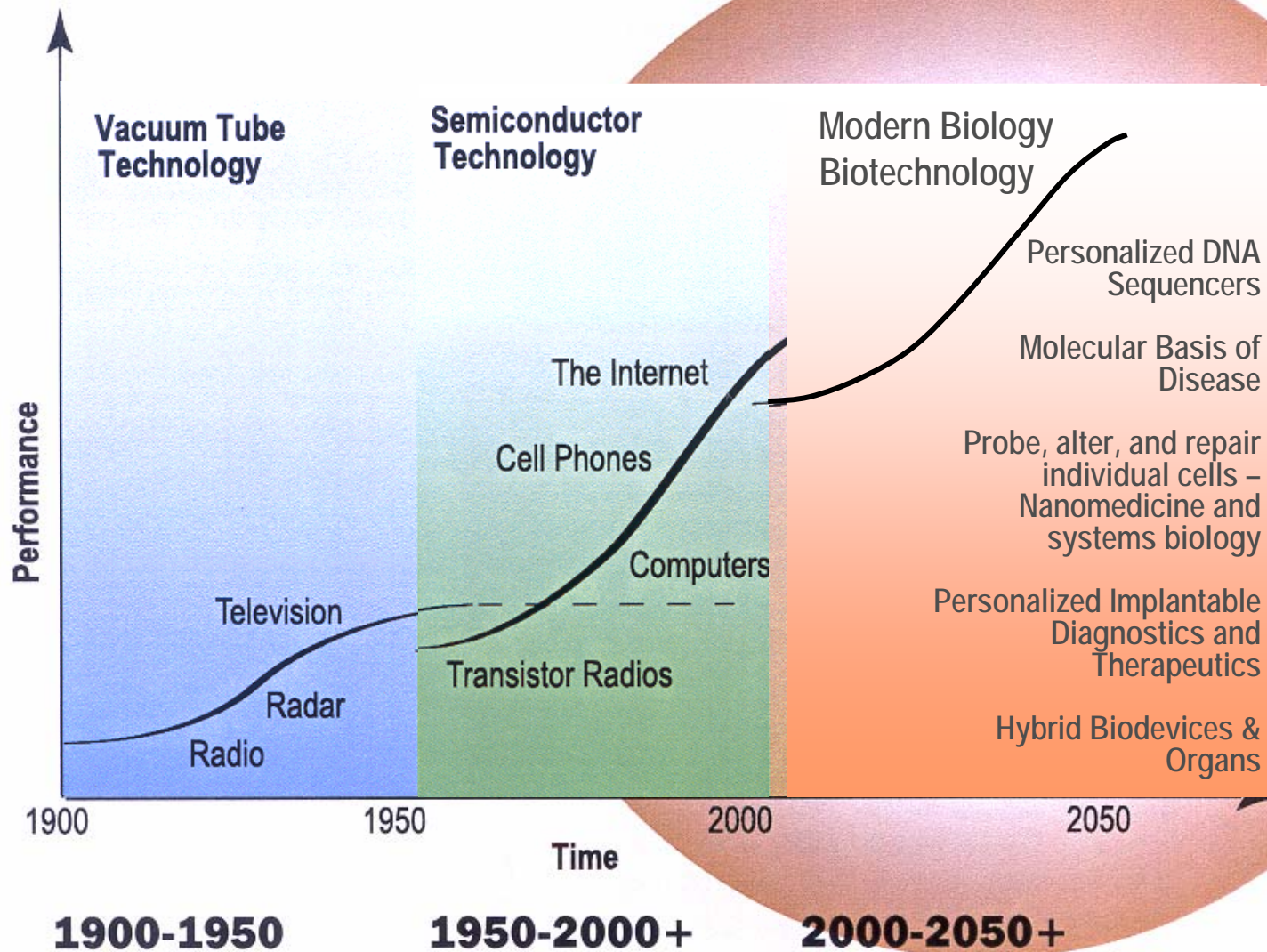


Microelectronic and  
MEMS

Nanoelectronics  
and Nanoscale  
Sensors



# Evolution of Technologies

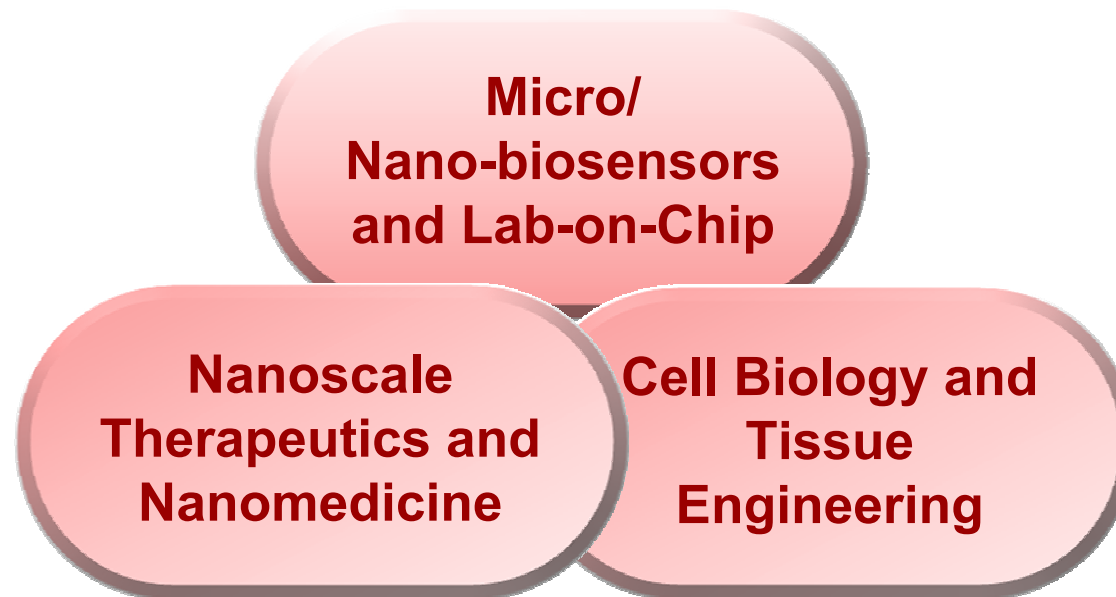






# Research Projects

- Petri dish on a chip with electrical detection
- Cantilevers for virus and bacterial detection
- Detection of CD4+ cells from blood
- Nanopores for single DNA molecule characterization
- Label free field effect silicon sensors for DNA and proteins



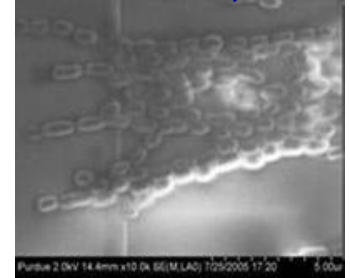
- Bacterial Mediated Delivery of Nanoparticles
- Macrophage Stealth Delivery of Nanovectors
- Phi-29 Nanomotor for Nanomedicine

- 3-D Tissue Engineering with Stereo-Lithography
- Nanomechanics for Cell Biology



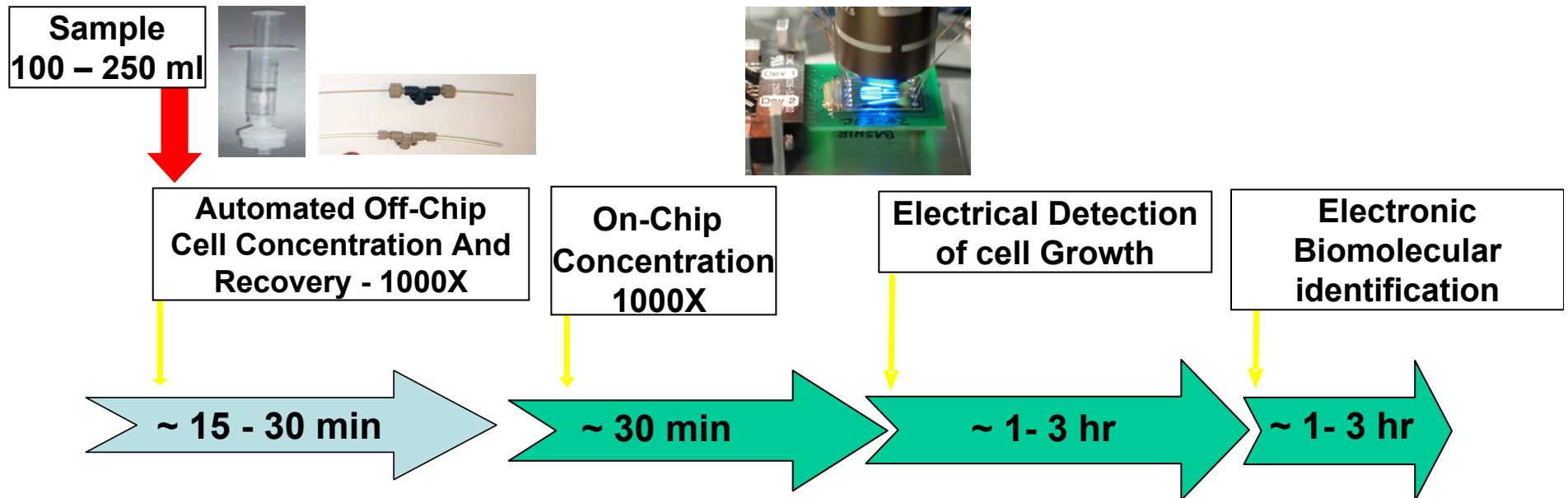
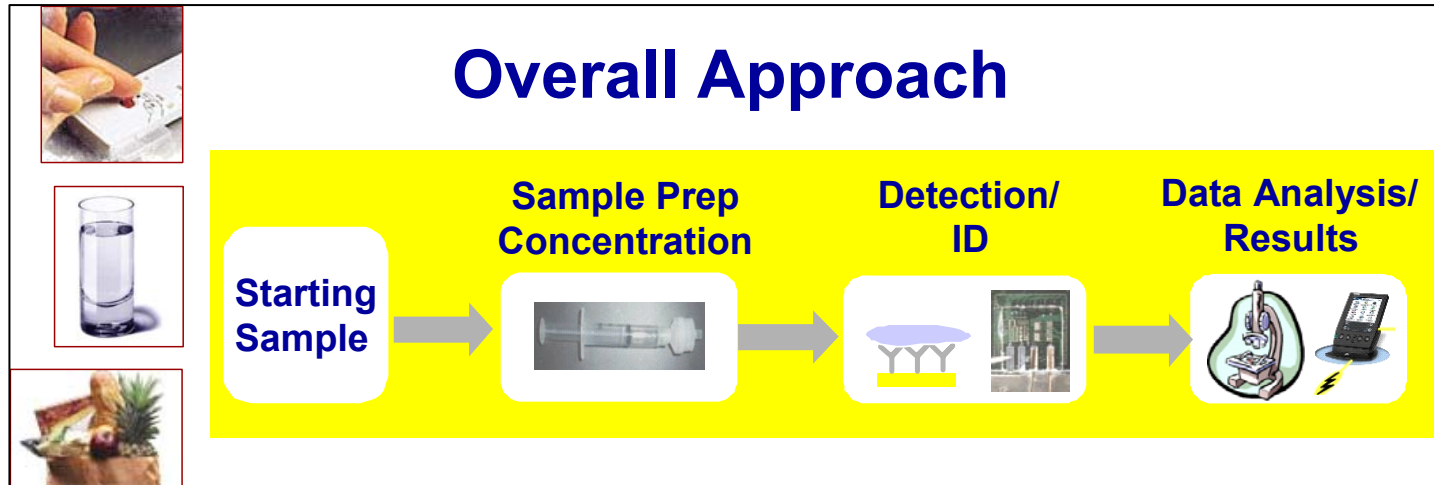
# Microfluidic-based technology platforms for bacterial detection

*L. Monocytogenes  
On a chip*



R. Bashir, ECE, BME  
A. Bhunia, Food Science  
M. Ladisch, BME, ABE  
J. P. Robinson, BMS, BME

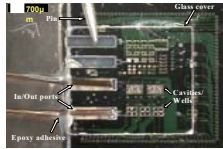
- **Rapid detection of live bacteria has wide applications**
  - Industrial Microbiology (Pharmaceutical facility monitoring, Food Safety)
  - Blood transfusion
  - Human Diagnostics
  - Global Health
- **Rapid time to result limited by:**
  - Amplification, enrichment, culture
  - 48-72 hours for growth and identification
- **Center for Food Safety Engineering at Purdue**  
([www.cfse.purdue.edu](http://www.cfse.purdue.edu)) through cooperative agreement with USDA-ARS



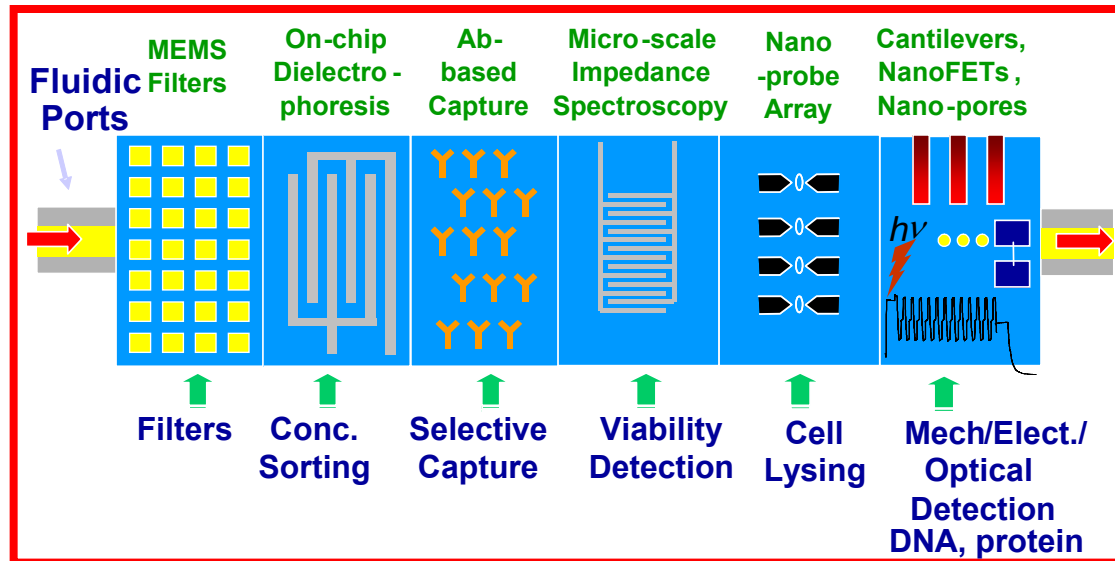
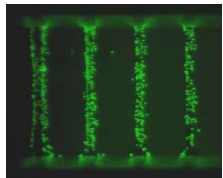


# Integrated Chips for Study of Microorganisms and Cells

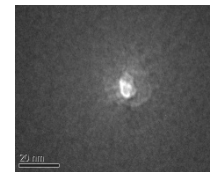
**Lab-on-a-chip for Detection of Live Bacteria**  
Liu, Park, Li, Huang, Geng, Bhunia, Ladisch, Bashir



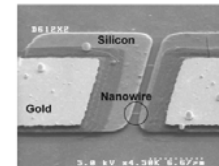
**Dielectrophoresis Filters and Traps for Biological Entities**  
Li, Akin, Bhunia, Bashir



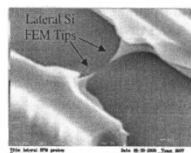
**Nanopore Sensors for DNA Detection**  
Chang, Andreadakis, Kosari, Vasmataz, Bashir



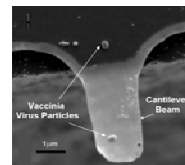
**Silicon Nanowires and Nanoplates for DNA and Protein Detection**  
Elilol, Reddy, Nair, Bergstrom, Alam, Bashir



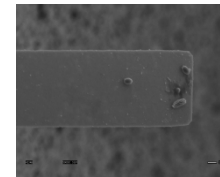
**Trapping/Lysing of Bacteria/Viruses In Microfluidic Devices**  
Park, Akin, Bashir



**Nano-Mechanical Cantilever Sensors for Detection of Viruses**  
Gupta, Akin, Broyles, Ladisch, Bashir



**Micro-Mechanical Cantilevers for Detection of Spores**  
Davila, Walter, Aronson, Bashir

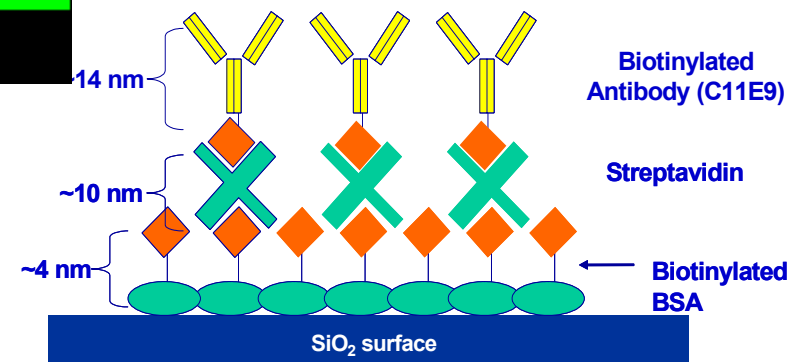
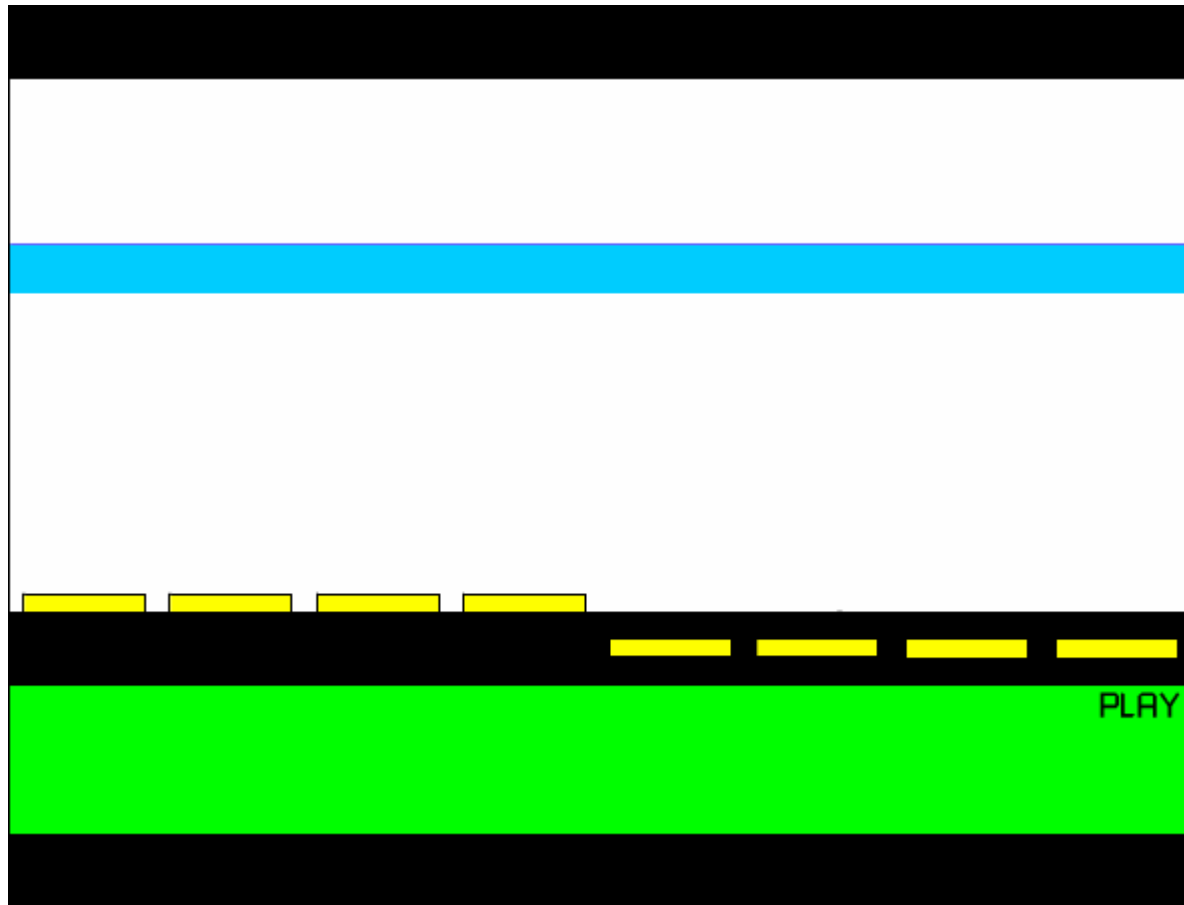


**“Lab on a Chip” with microfluidics and micro/nanosensors**





# Overall Detection Scheme

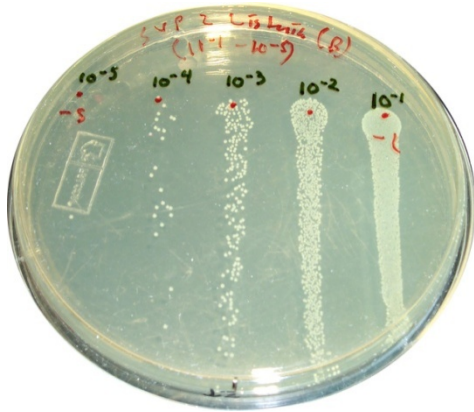


*Gomez, Morisette, Bashir, IEEE/ASME JMEMS, 2005*  
*Yang, Li, Akin, Huang, Bhunia, Ladisch, Bashir, Lab Chip, 2006*

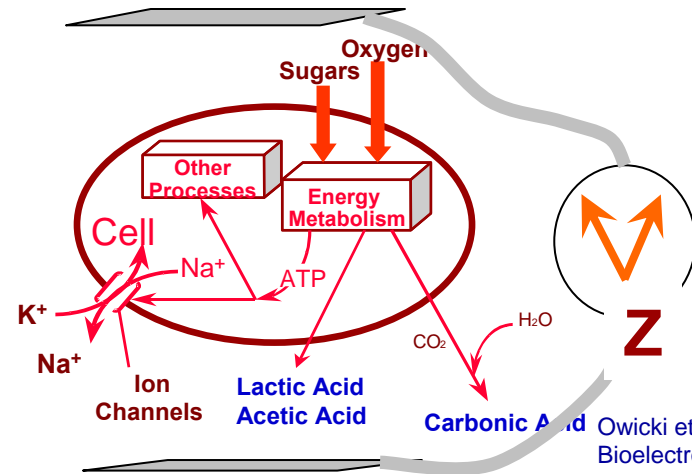
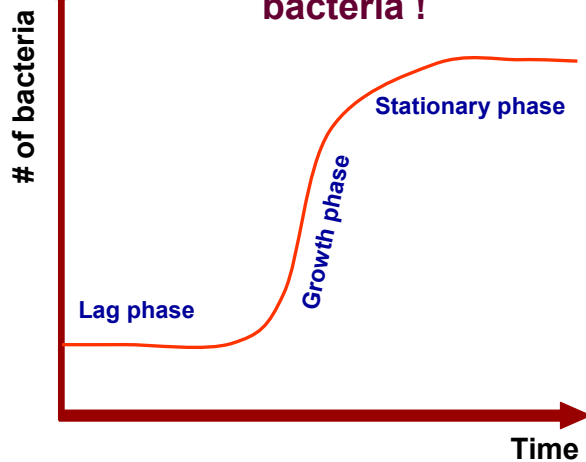
\* Size information are obtained from Biochemistry 2<sup>nd</sup> 9  
edition, R. H. Garrett and C. M. Grisham, 1995.



# Bacterial Growth & Impedance Microbiology !

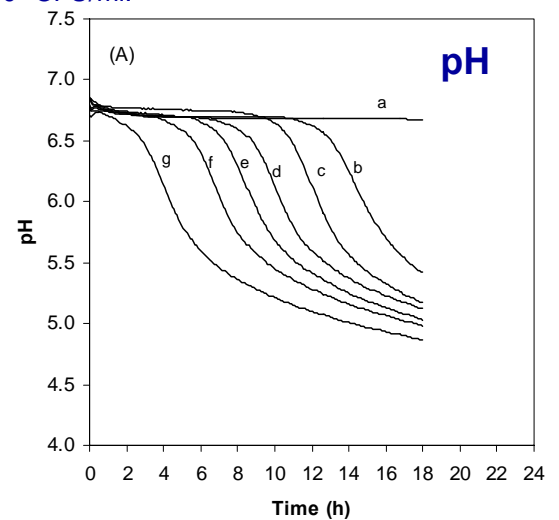
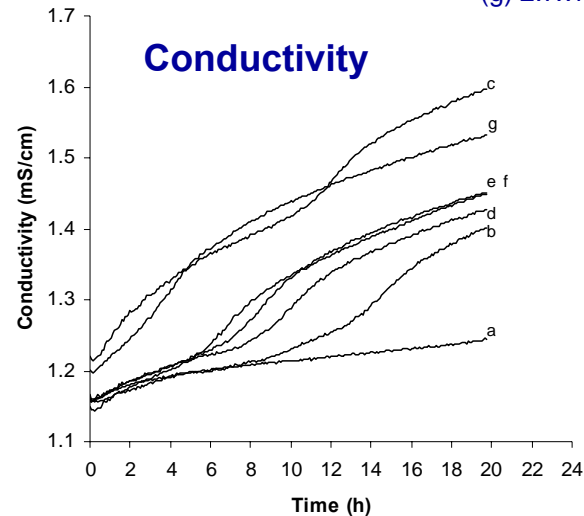


Invented in late 1800s (Petri and Koch)  
Still the most widespread means to  
grow and detect the presence of  
bacteria !



Owicki et al., Biosens. Bioelectron. (1992)

(a) no cell, (b)  $2.5 \times 10^2$ , (c)  $2.39 \times 10^3$ , (d)  $2.64 \times 10^4$ , (e)  $2.66 \times 10^5$ , (f)  $2.65 \times 10^6$ , (g)  $2.7 \times 10^7$  CFU/ml.

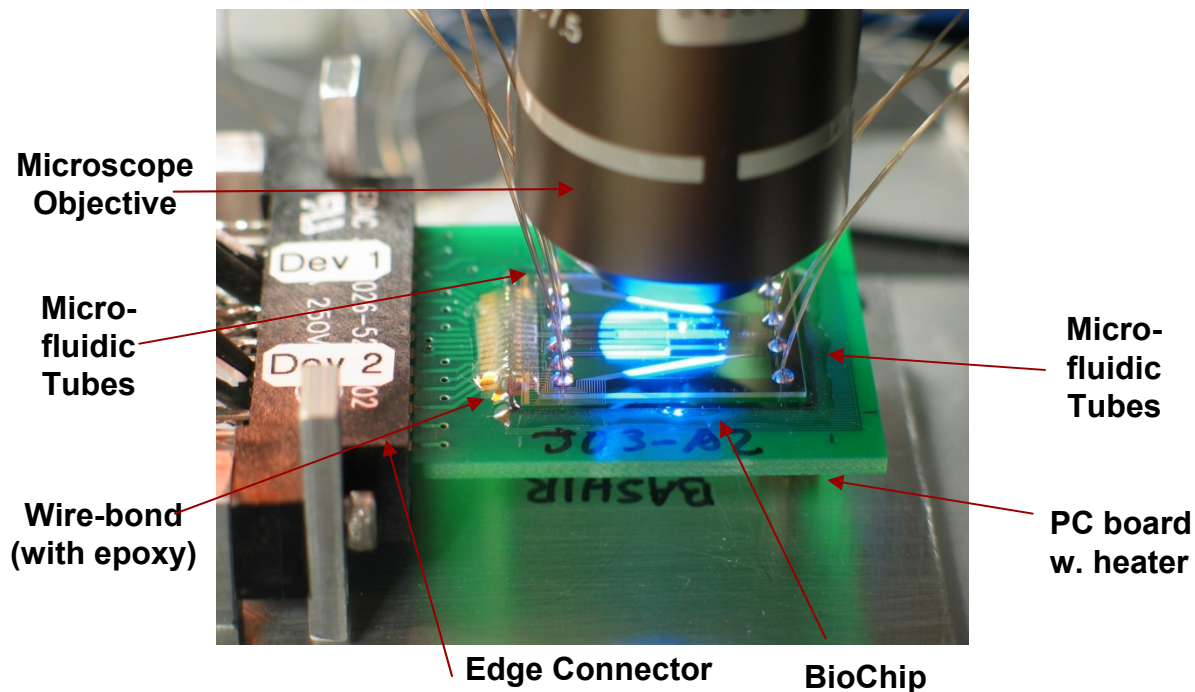
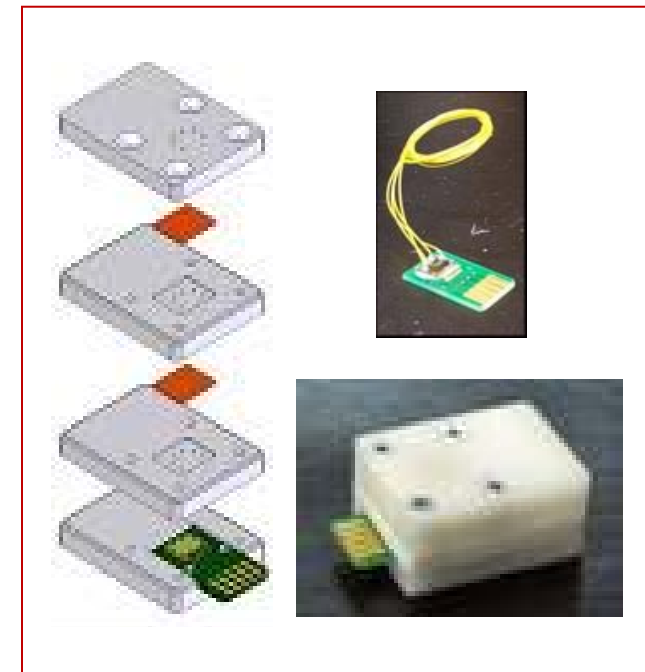
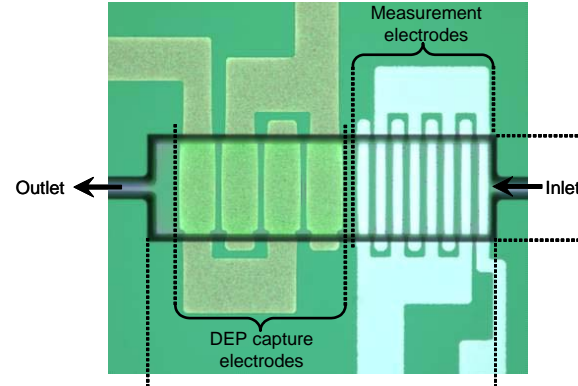
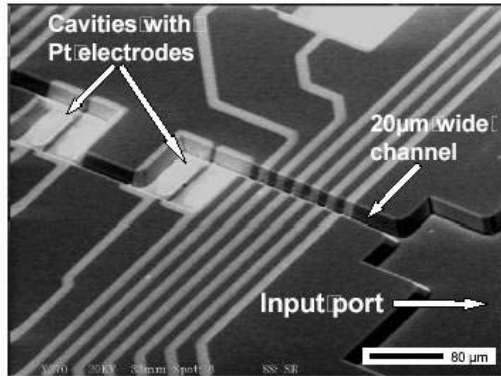


10

Yang, L, Banada, P., Bhunia, A. Bashir, R., Biotech Bioengr, 2005



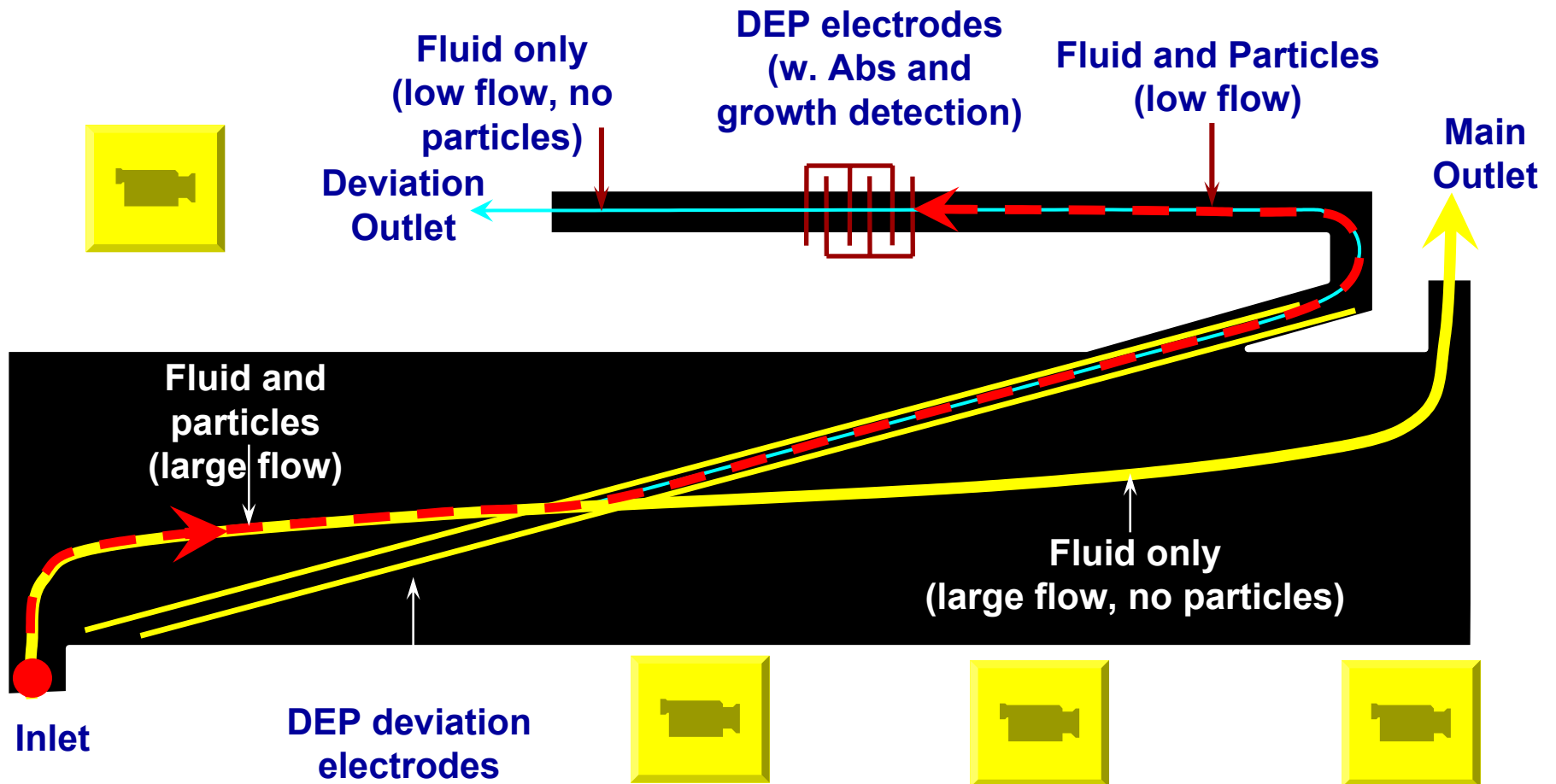
# Petri Dish-on-a-Chip





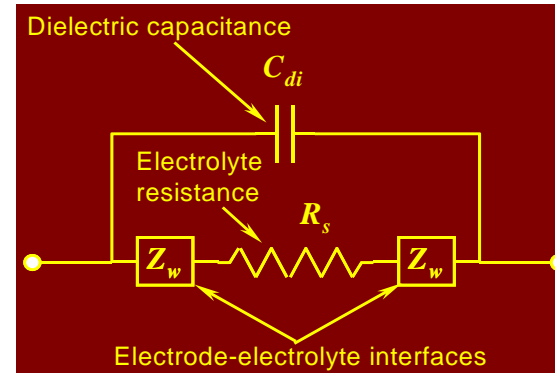
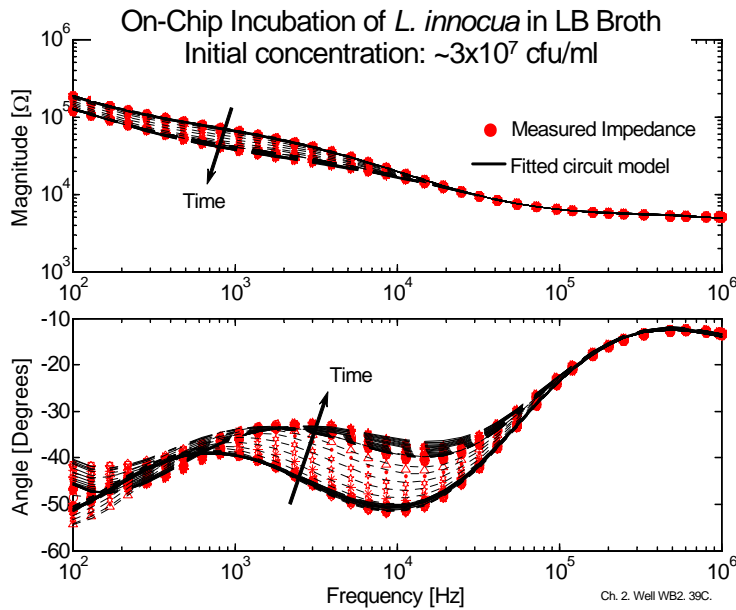
# Bacterial Cell Concentration on-Chip

- DEP-based concentration system collects particles from a large flow stream and diverts them to a smaller stream





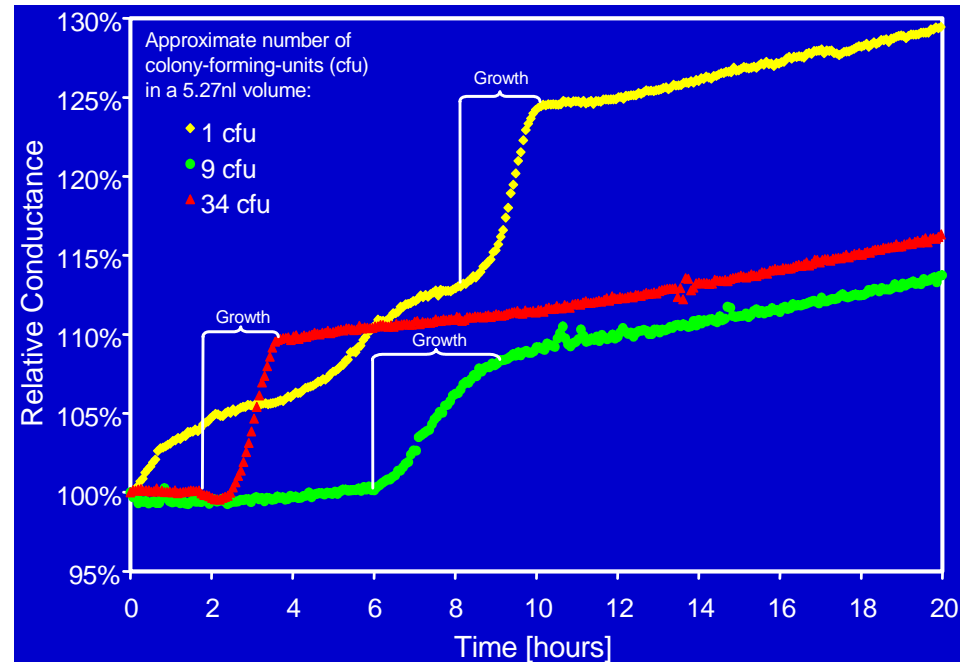
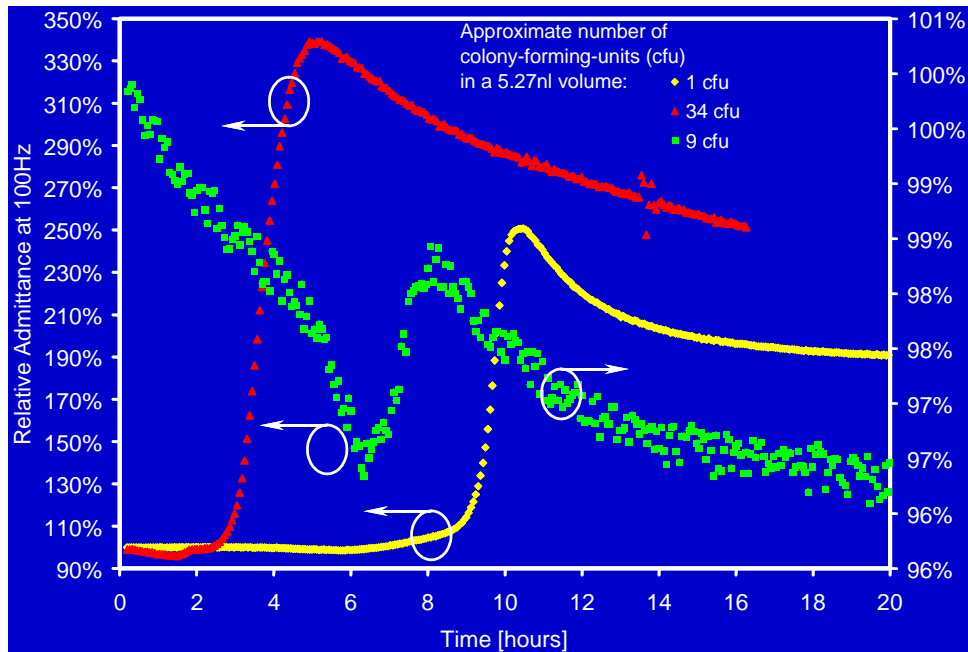
# On-Chip Incubation of *L. Monocytogenes*



**Electrode-Electrolyte Interface Model:**

$$Z_w = \frac{1}{(j\omega)^n B}$$

**Constant-angle impedance**



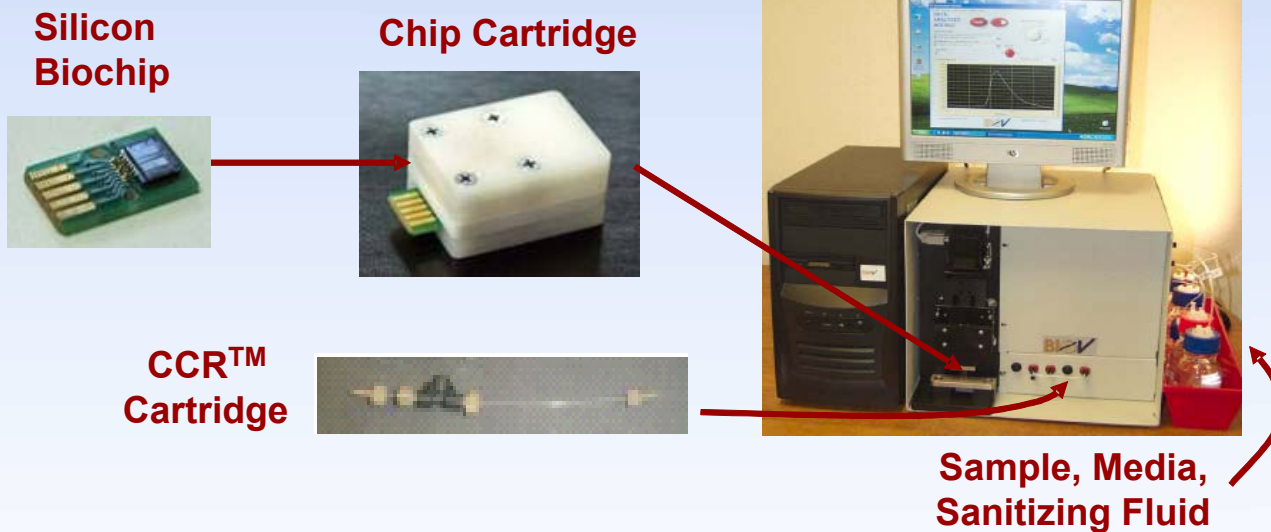




# BioVitesse, Inc.

- 'Petri dish on a chip' to miniaturize impedance microbiology
- To quickly and reliably detect and identify *live bacteria* in 2 to 4 hours, instead of 2 to 10 days
- Provides in-process quality control monitoring systems
- To the industrial microbiological market (Bio/Pharma and Food Safety)

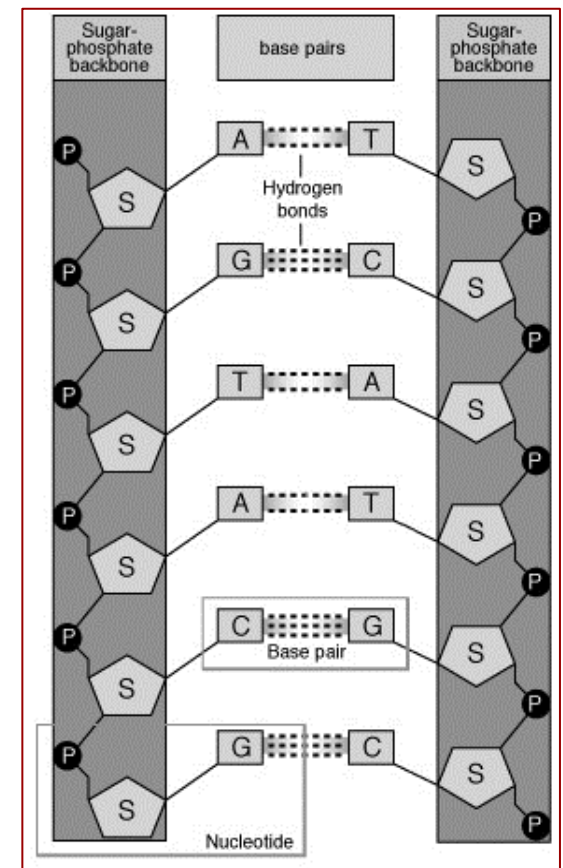
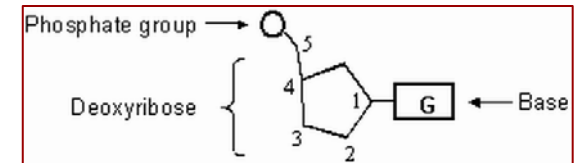
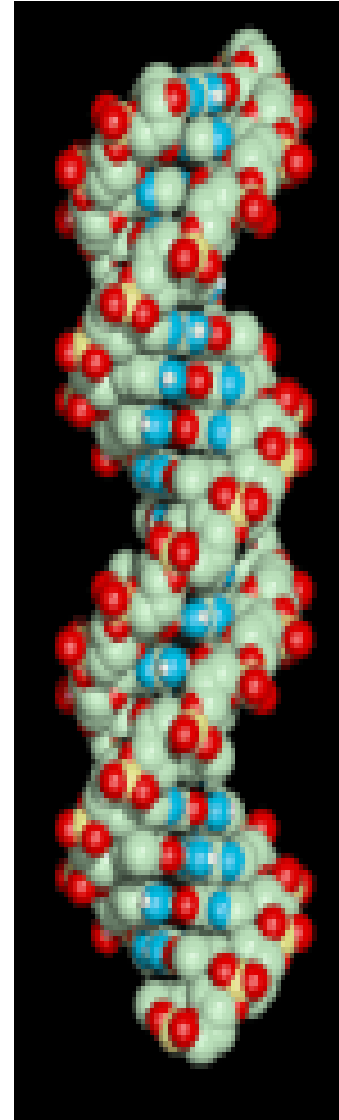
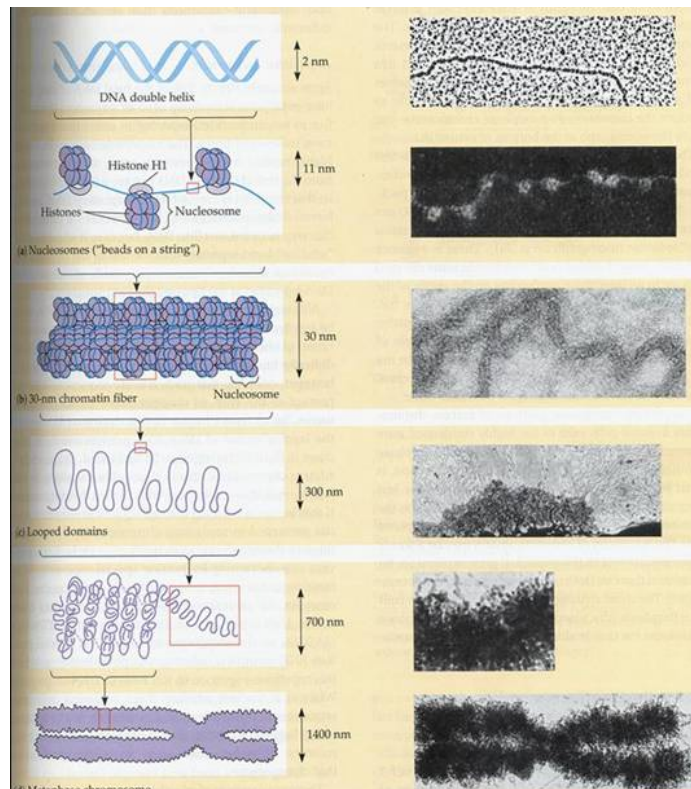
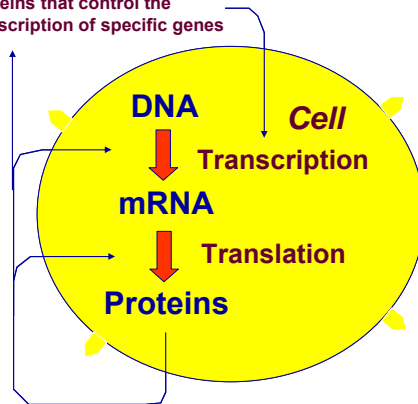
## Automated System





# DNA – the code of life in all Cells!

Transcription factors:  
Proteins that control the  
transcription of specific genes

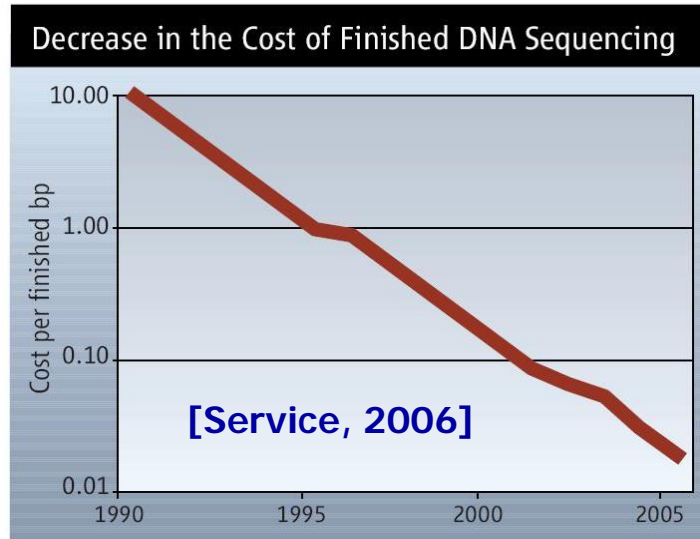


<http://www.chromosome.com/dna.html>

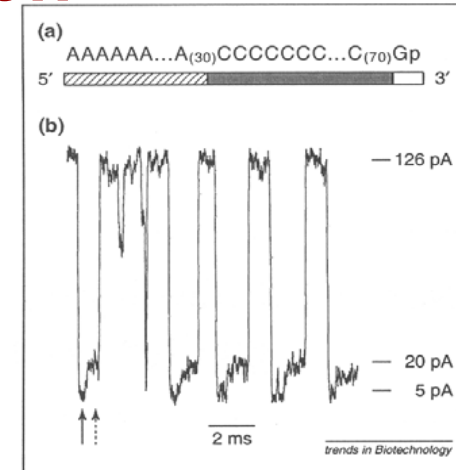


# Nanopores for single DNA molecule characterization

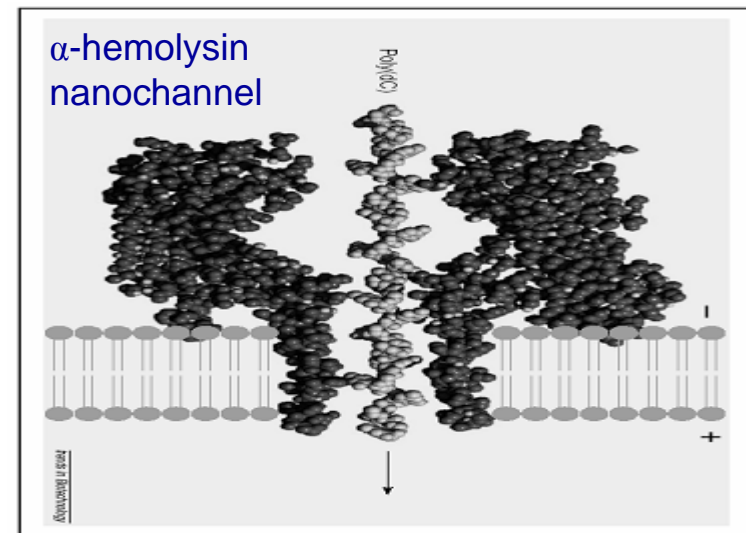
$$2\text{c/bp} \times 3\text{e9bp} = \$60\text{M} !$$



- $\alpha$ -hemolysin channel, a biological protein based-pore
- Diameter of 2.6 nm.
- Translocation of ssDNA using electrophoresis
- Nanoscale coulter counter



Poly-A  
Poly-C



The model of DNA passing through an  $\alpha$ -hemolysin channel.



# Nanopore Fabrication

## Key steps

- EBL to write dots
- TMAH etch
- Pore in SOI
- Oxidation
- Shrinking in TEM

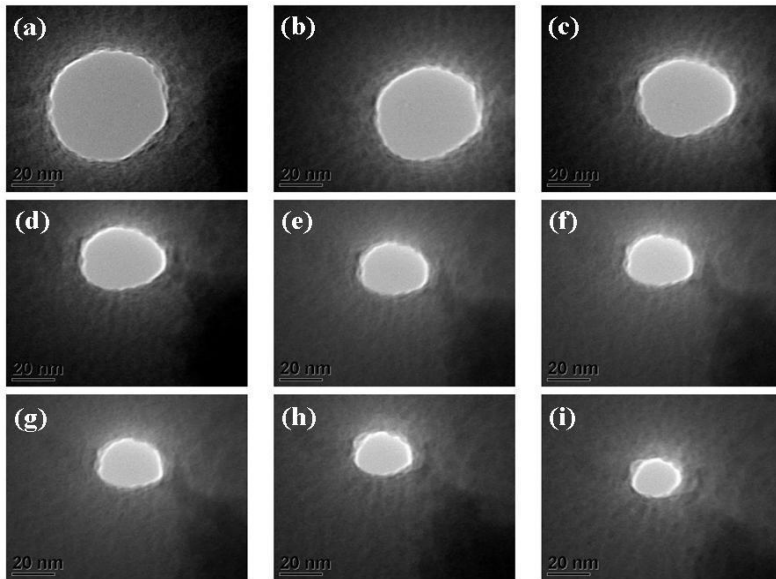
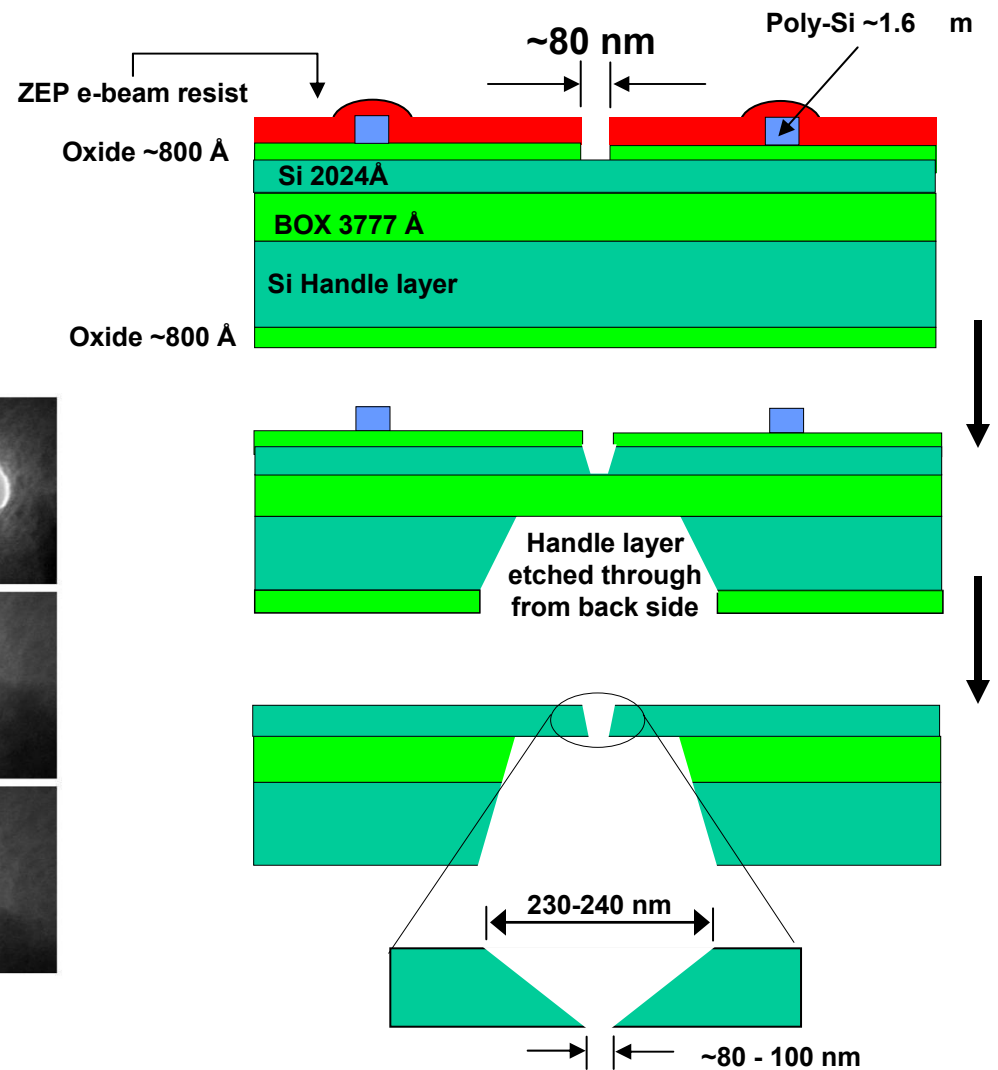


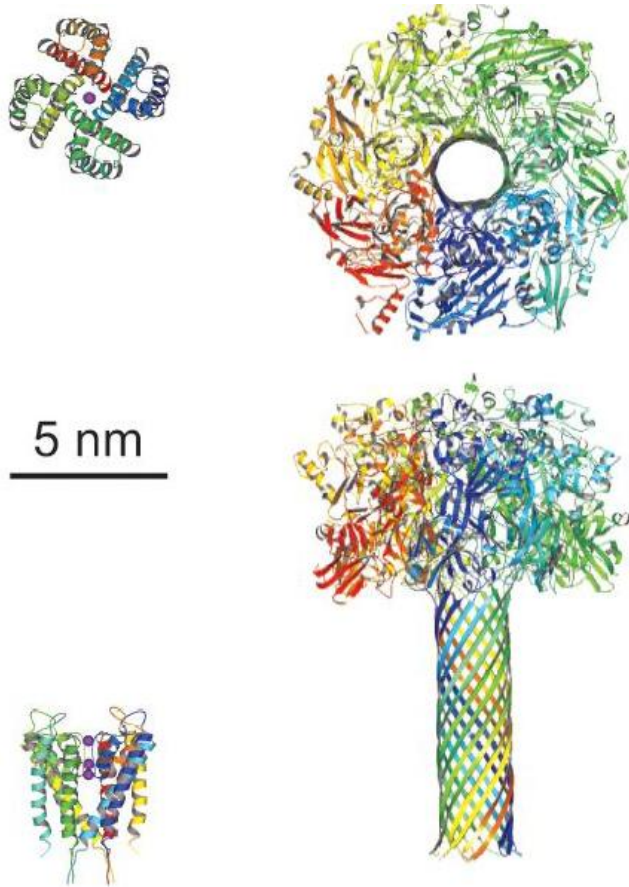
Figure 1. Pore shrinking temporal profile of a nanopore channel  
All Images at 1,000,000X. (NPC-2)





# Adding DNA Selectivity to Solid State Nanopores

## Protein Ion Channels

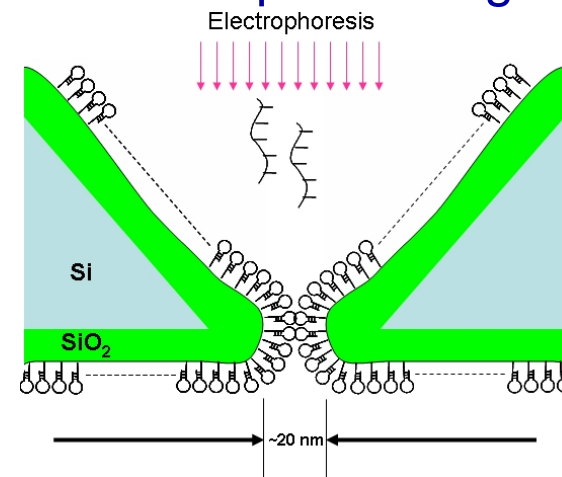


K<sup>+</sup> channel

PA<sub>63</sub> channel

[Kasianowicz *et al.*, 2006]

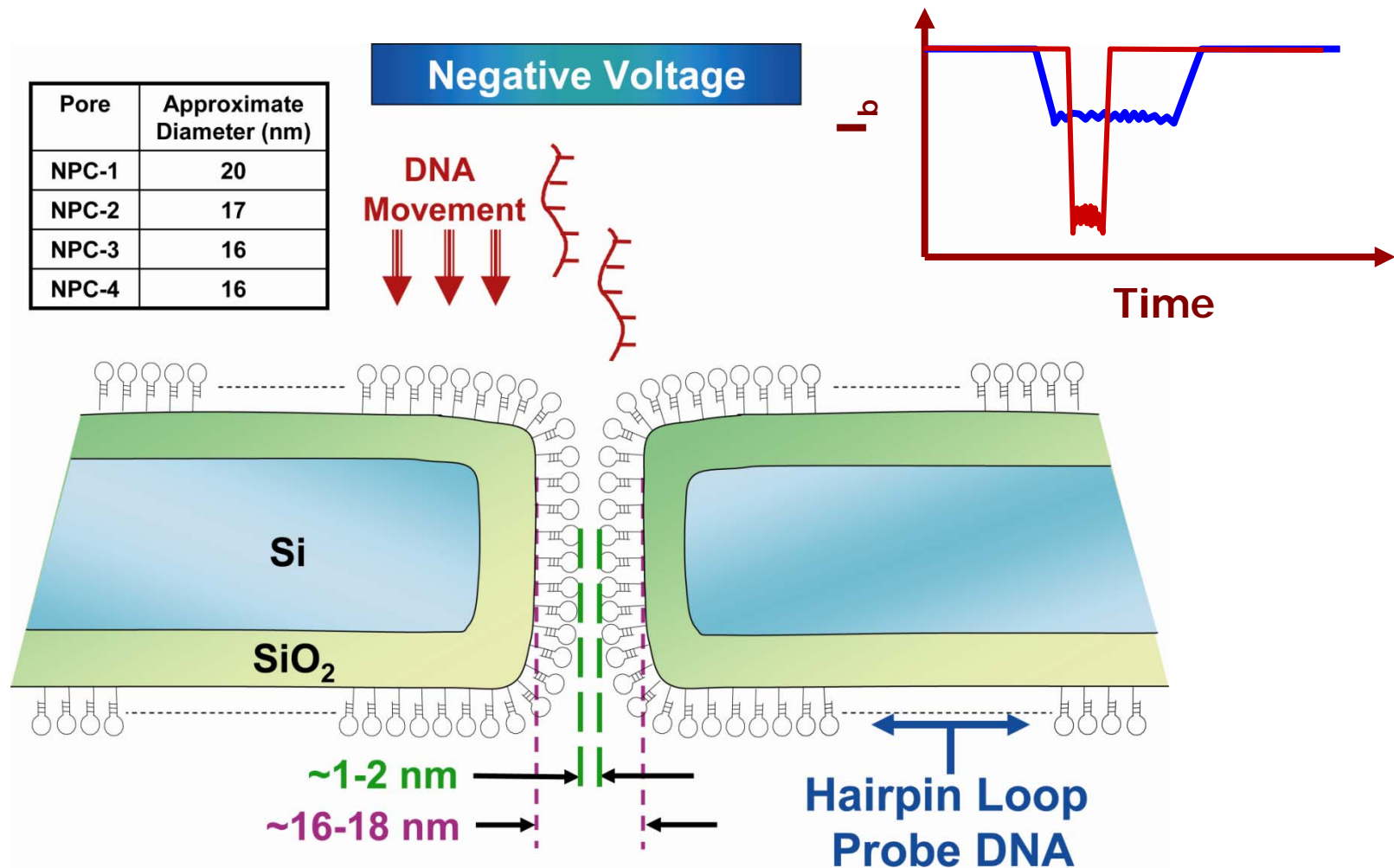
## Nanopores with selectivity towards specific targets



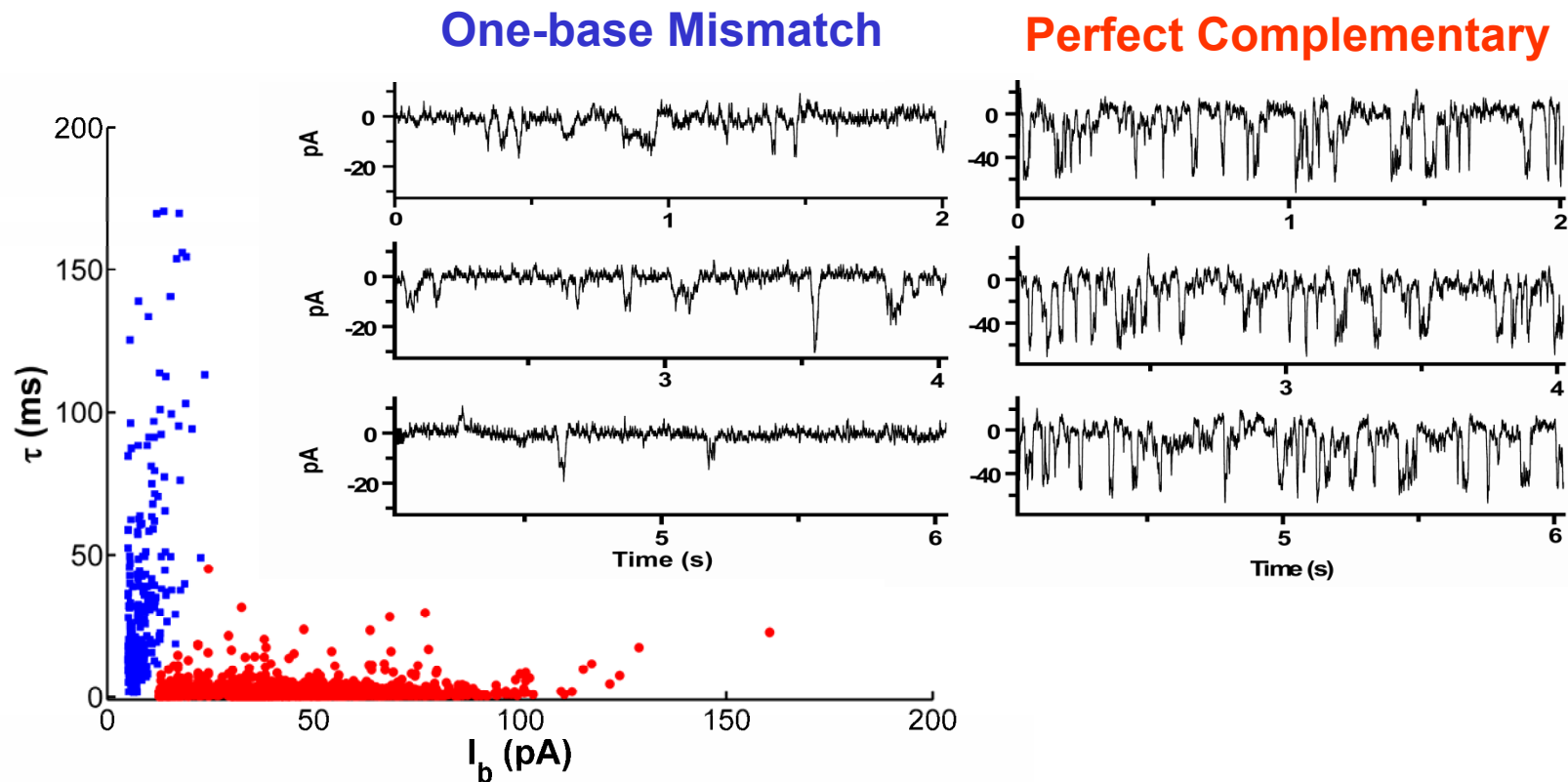




# Selective Nanopores Measurements Overview

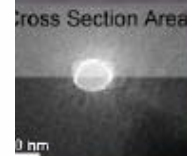


Courtesy of  
Seyet, LLC



NPC-1	1MM-DNA (in 120 min)		PC-DNA (in 120 min)		1MM-DNA after PC-DNA (in 120 min)	
Signature of pulses	$\tau$ (ms)	$I_b$ (pA)	$\tau$ (ms)	$I_b$ (pA)	$\tau$ (ms)	$I_b$ (pA)
Mean	178.8	28.9	10.2	31.2	92.0	29.1
Sigma	260.3	31.7	30.4	27.8	78.2	23.0
Number of pulses	3,353		96,876		2,896	

Si

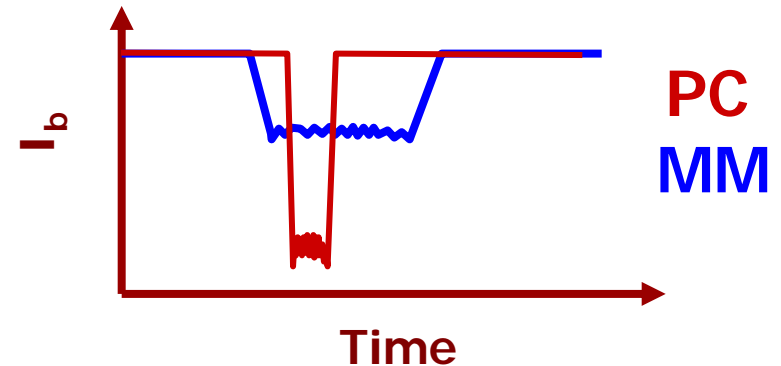


SELECTIVE TRANSPORT  
MOLECULES THROUGH  
SOLID-STATE NANOPORE CHANNELS



# Single-Base Mismatch Selectivity

- Channel-Molecular Interaction
  - MM-DNA vs. PC-DNA
- PC-DNA
  - Interactions with Binding Sites
  - Faster and More than MM-DNA
- MM-DNA
  - Electrostatic Friction
  - Mechanical Resistance
  - Inability to open HPL



$$J = \frac{n}{\tau} (c_1 - c_2)$$





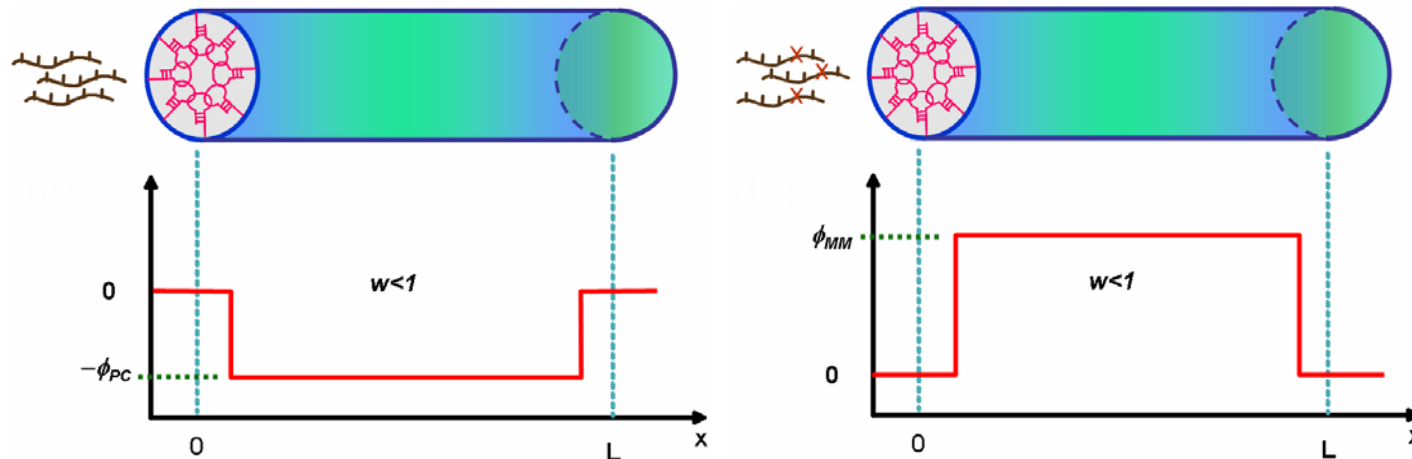
# Channel Interaction

## Attractive vs. Repulsive Potential

### Key Assumptions

- PC/HPL: Attractive Potential
- MM/HPL: Repulsive Potential
- Magnitudes of Potentials
- $\phi$  span part of the channel

$$\frac{\tau_{MM}}{\tau_{PC}} = e^{|\phi_{MM}| - |\phi_{PC}|}$$

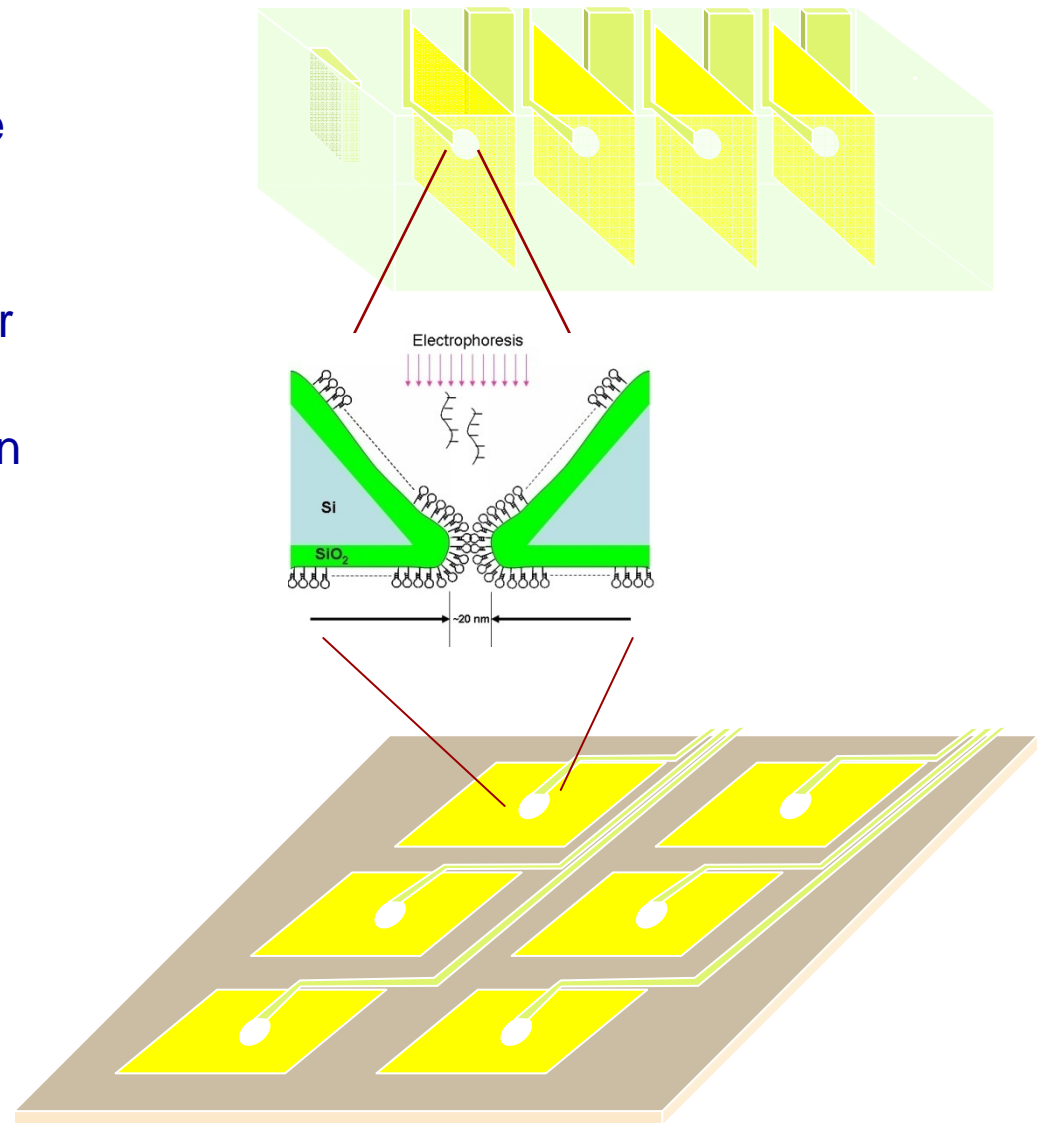


(a) Attractive potential (b) Repulsive potential, spanning part of the channel



# Nanopore Channel Sensor Array for Characterization of Single Molecules

- Miniature DNA analyzer
  - Transduction events at single molecule, nanoscale
  - Interface to the macroscale
  - Array of nanopores – serial or parallel ?
  - Site selective functionalization strategy
- Sequencing by digestion
  - Smaller molecules – bases !
  - Digest and detect







# Microcantilever Mass Sensors

Unloaded Resonant Frequency :

$$f_0 = \frac{1}{2\pi} \sqrt{\frac{k}{m^*}}$$

Spring constant for a rectangular shaped cantilever beam:  $k = \frac{Et^3w}{4l^3}$

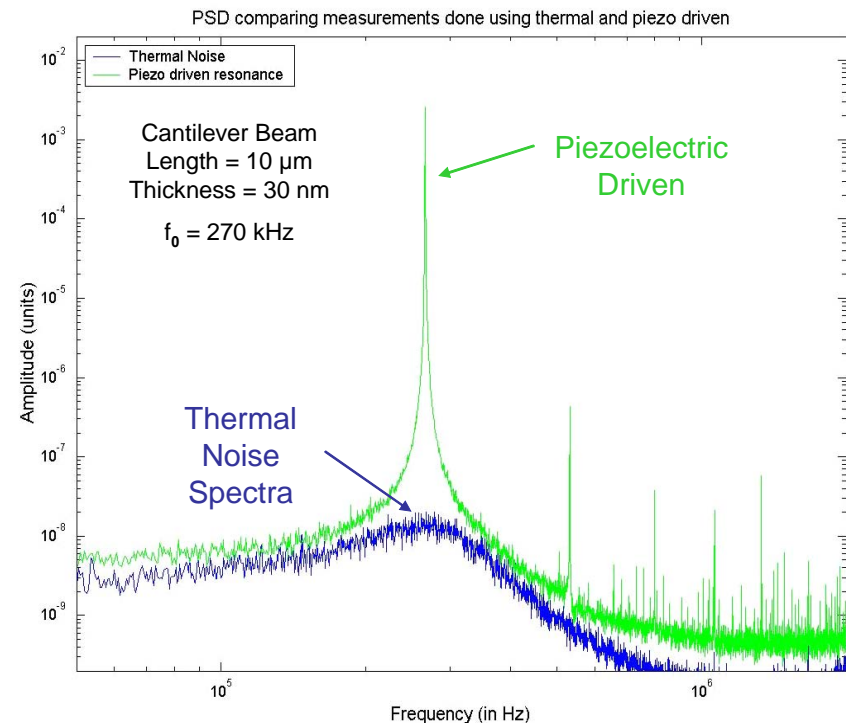
Loaded Resonant frequency :  $f_1 = \frac{1}{2\pi} \sqrt{\frac{k}{m^* + \delta m}}$   
 $\delta m$  is the added mass

$$\Delta m = \frac{k}{4\pi^2} \left( \frac{1}{f_1^2} - \frac{1}{f_0^2} \right)$$

- $k$  = spring constant
- $m$  = mass of cantilever
- $f_0$  = *unloaded resonant frequency*
- $f_1$  = *loaded resonant frequency*

24

## Mass Change Detection





# Nanomechanical Sensors for Viral Detection

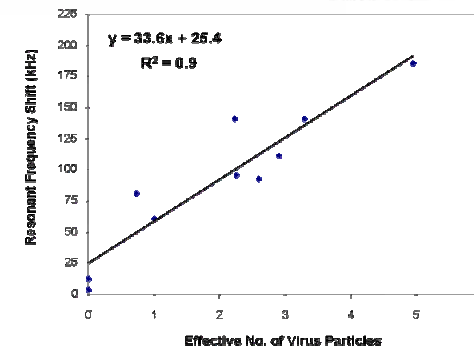
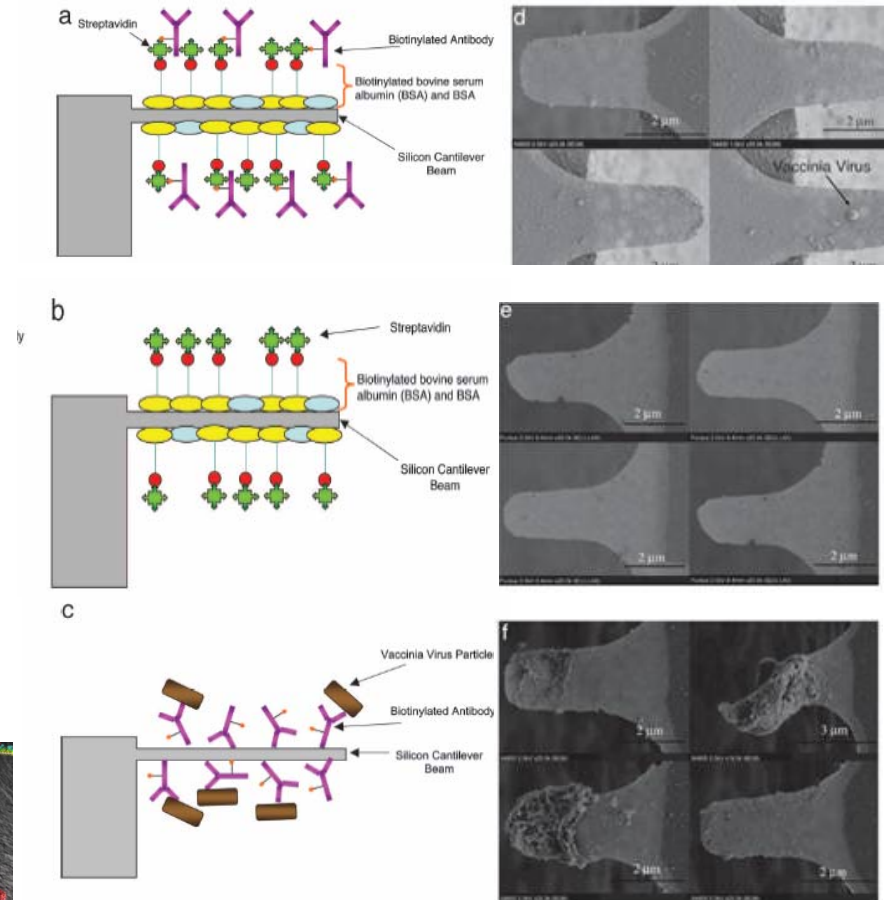
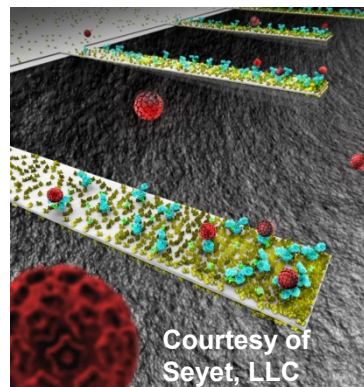
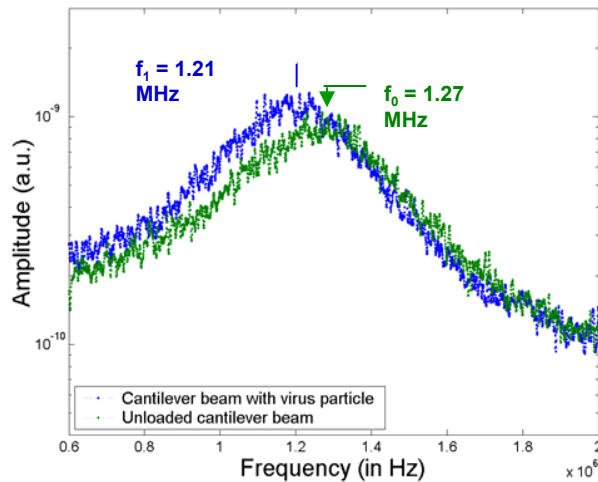
## Objectives:

To develop technology for the rapid detection of virus particles in fluid and air using Nanomechanical Cantilever Sensors

Frequency Shift,  $\Delta f = 60$  kHz

⇒ Mass change,  $\Delta m = 9$  fg

⇒ This corresponds 1 vaccinia virus.

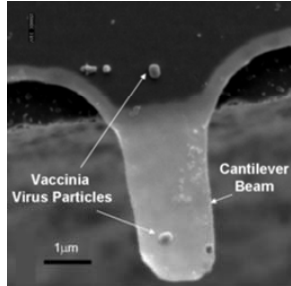




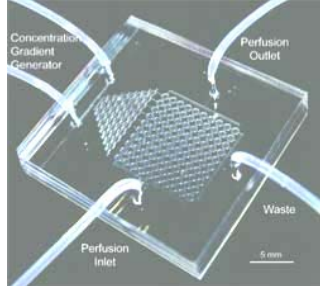
# Living Cantilever Arrays

Measuring the growth-rate of a single cell,  
under various combination of stimuli.

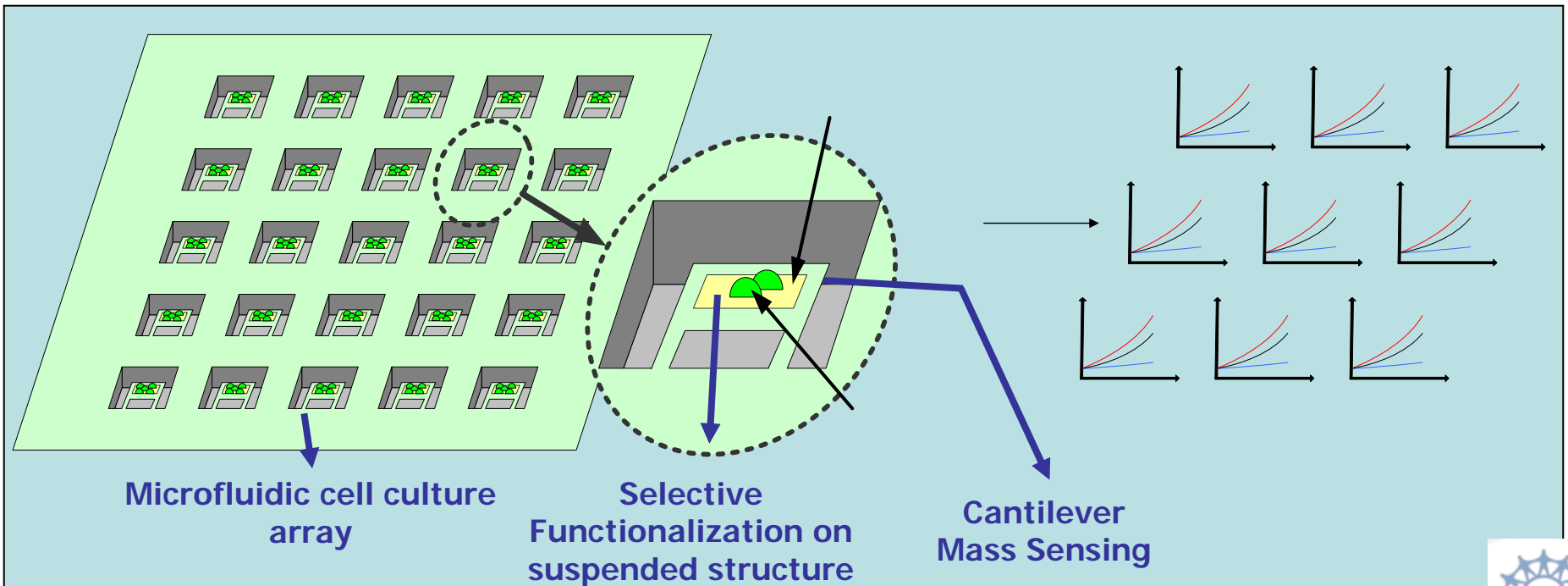
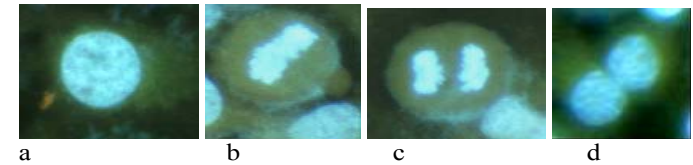
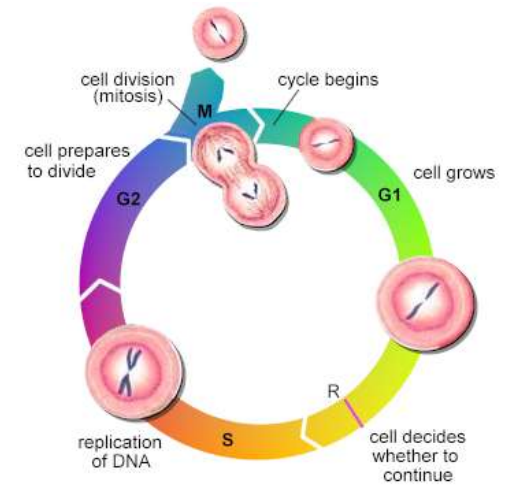
Cantilever mass sensing



μ-fluidic cell culture array



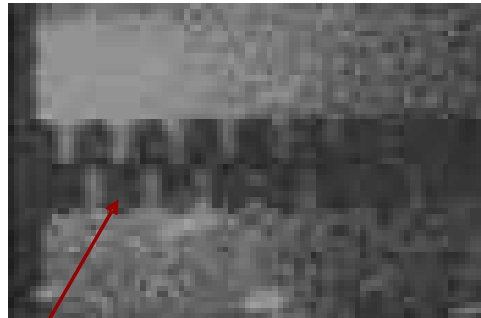
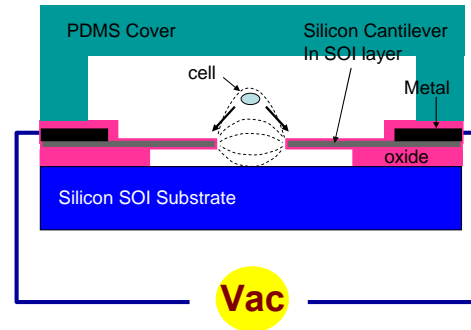
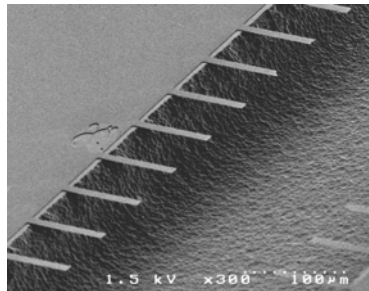
L. P. Lee (UCB)





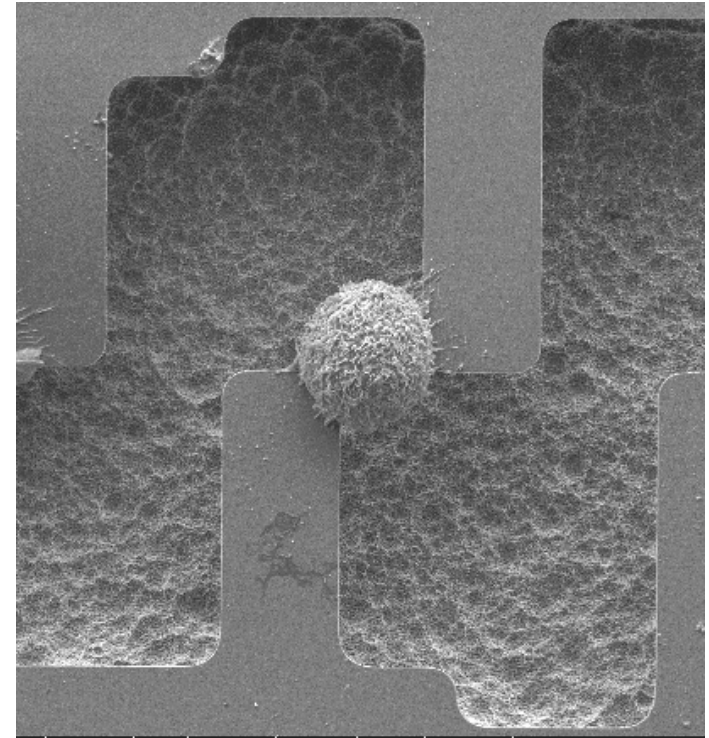
# Cell Attachment on Cantilevers

- DEP Assisted Capture



DEP Off

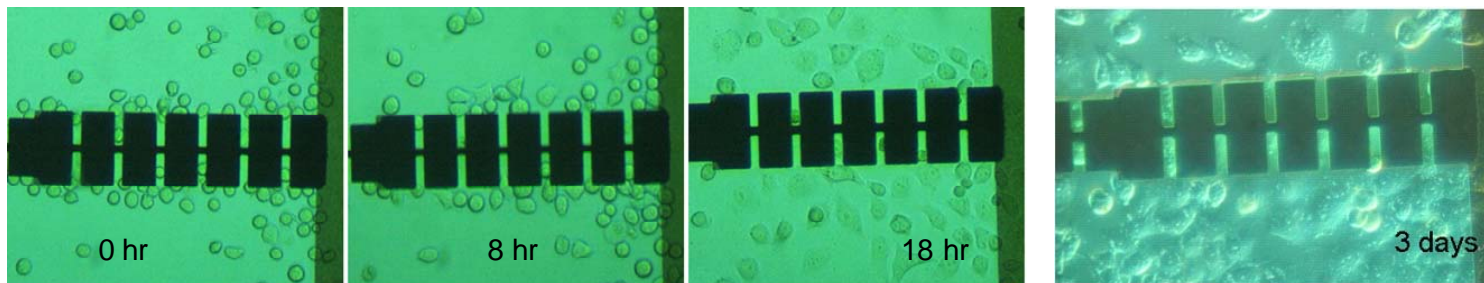
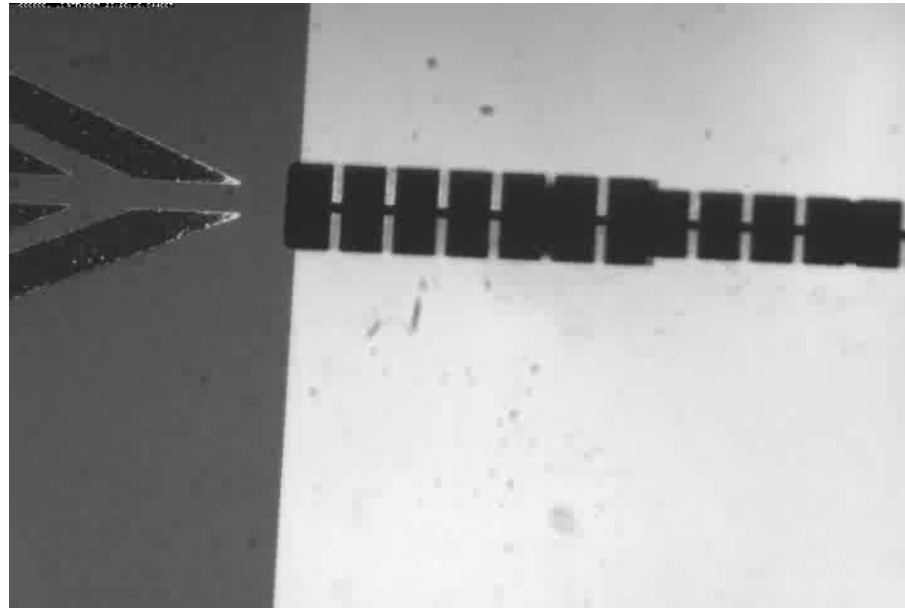
DEP On



Hela cells, captured with DEP. Conductive silicon electrode generate DEP forces to capture Hela cells.



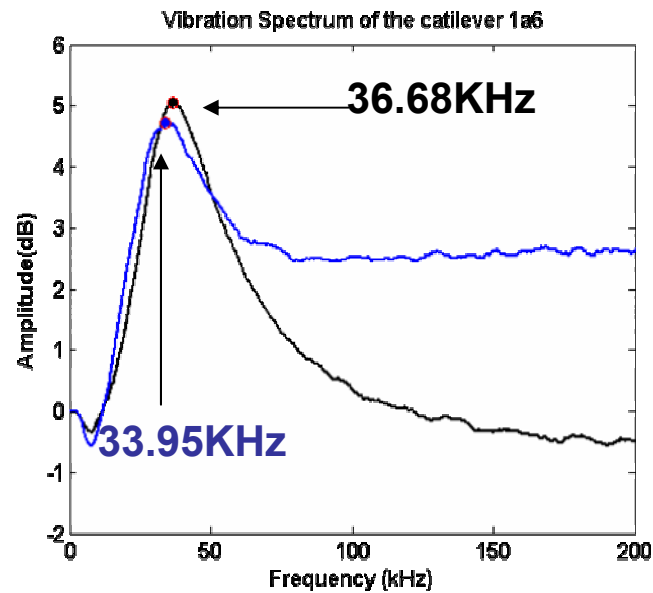
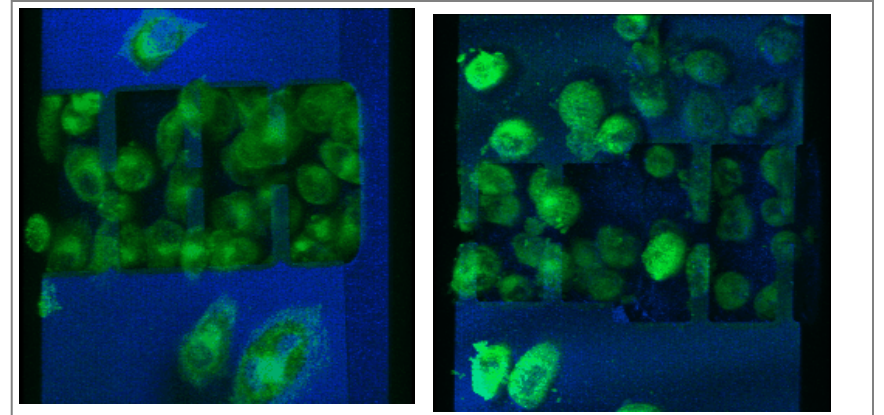
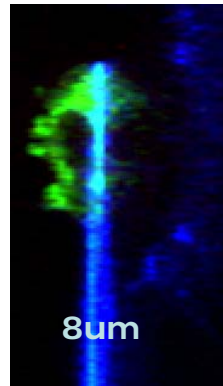
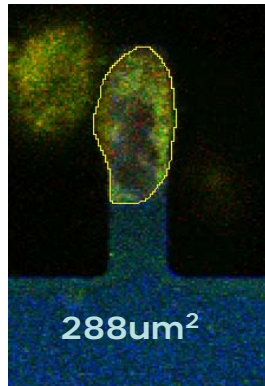
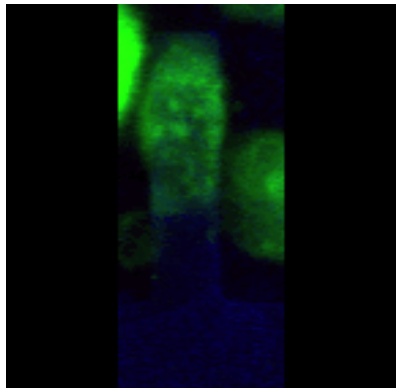
# Living Cantilever Arrays







# Living Cantilever Arrays



Calculated  
Mass: 2.06 ng

Volume: 2349  $\mu\text{m}^3$   
Density<sup>3</sup>: 1.055g/cc  
Estimated mass :  
2.48 ng



# Point of Test Biosensors

## Abbott/iSTAT (Glucose)

Precision Xtra<sup>®</sup>  
Blood Glucose & Ketone Monitoring System

For Simple, Everyday Testing

Simple 2-Step Testing  
Just insert strip and apply blood

Auto Calibration  
Simply insert calibrator into the strip port; no coding required

Simple Blood Application  
End-fill or top-fill, with visual confirmation

NOW with NEW, IMPROVED Test Strip!  
Fast 5-second test time and small 0.6 microliter sample size



## Accuteck (LDH, Theophylline)



## Abbott/iSTAT (gases, ions, markers)

Discover our complete family  
of i-STAT cartridges

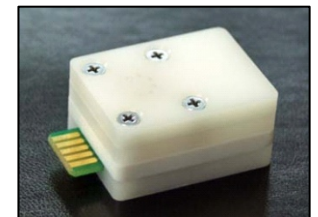
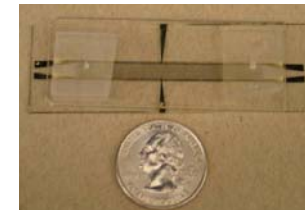
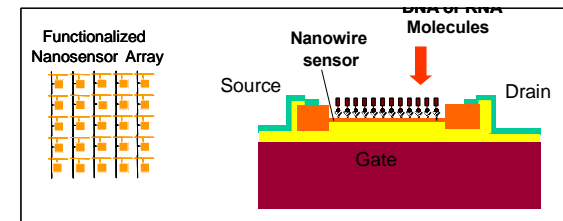
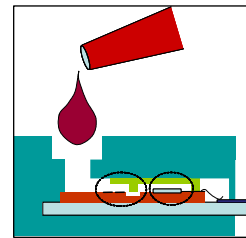


## Pregnancy Tests



## Silicon Based BioChips !

- Disposable, one-time-use devices
- Rapid, sensitive, integrated
- Detection and monitoring of disease and state of health

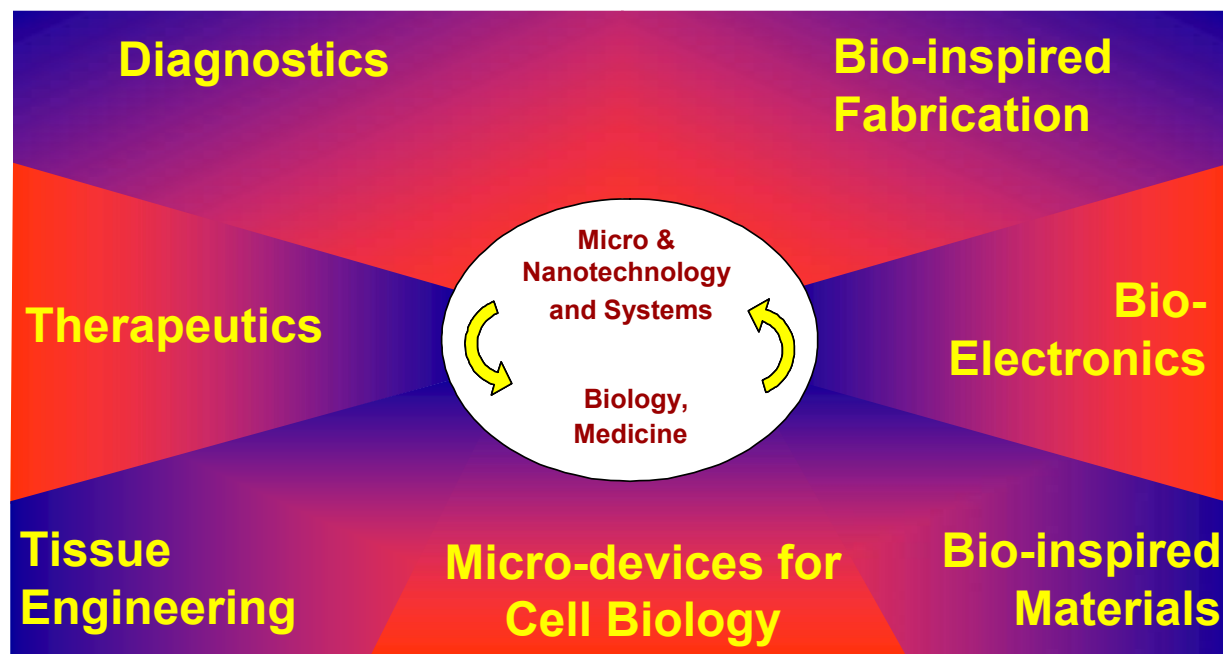


- Focus on translation: Top-down integrated nano-structures and nano-sensors platforms – POC sensors for biomolecules
- Chip makers and diagnostic industry
- System level fabrication and modeling/simulations (from 'molecules to systems') with considerations of integrated systems, fluid and biomolecule transport, packaging and interfaces, etc.



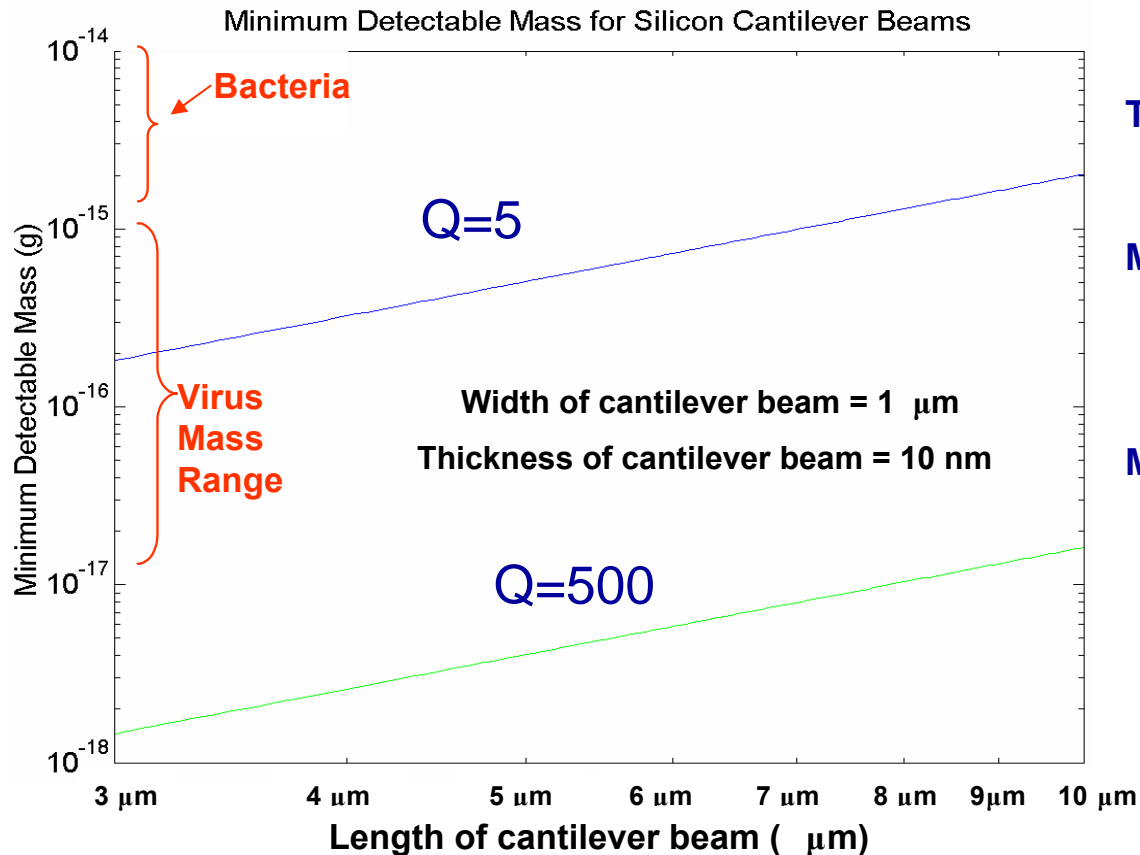
# BioMEMS and Bionanotechnology

Apply micro-systems and nanotechnology to develop novel devices and systems that have a biomedical impact or are bio-inspired





# Minimum Detectable Mass



100kDa Protein  $\sim 10^{-19}$  g

DNA bp  $\sim 10^{-21}$  g

The frequency measurement is limited by thermo-mechanical noise on the cantilever beam.

Minimum Detectable Frequency,

$$\Delta f_{\min} = \frac{1}{A} \sqrt{\frac{f_0 k_B T B}{2 \pi k Q}}$$

Minimum Detectable Mass,

$$\Delta m_{\min} = \frac{1}{A} \sqrt{\frac{4 k_B T B}{Q}} \frac{m_{\text{eff}}^{5/4}}{k^{3/4}}$$

$k_B$  = Boltzmann constant

T = Temperature in Kelvin

B = Bandwidth measurement, ( $= 2\pi f_0/2Q$ )

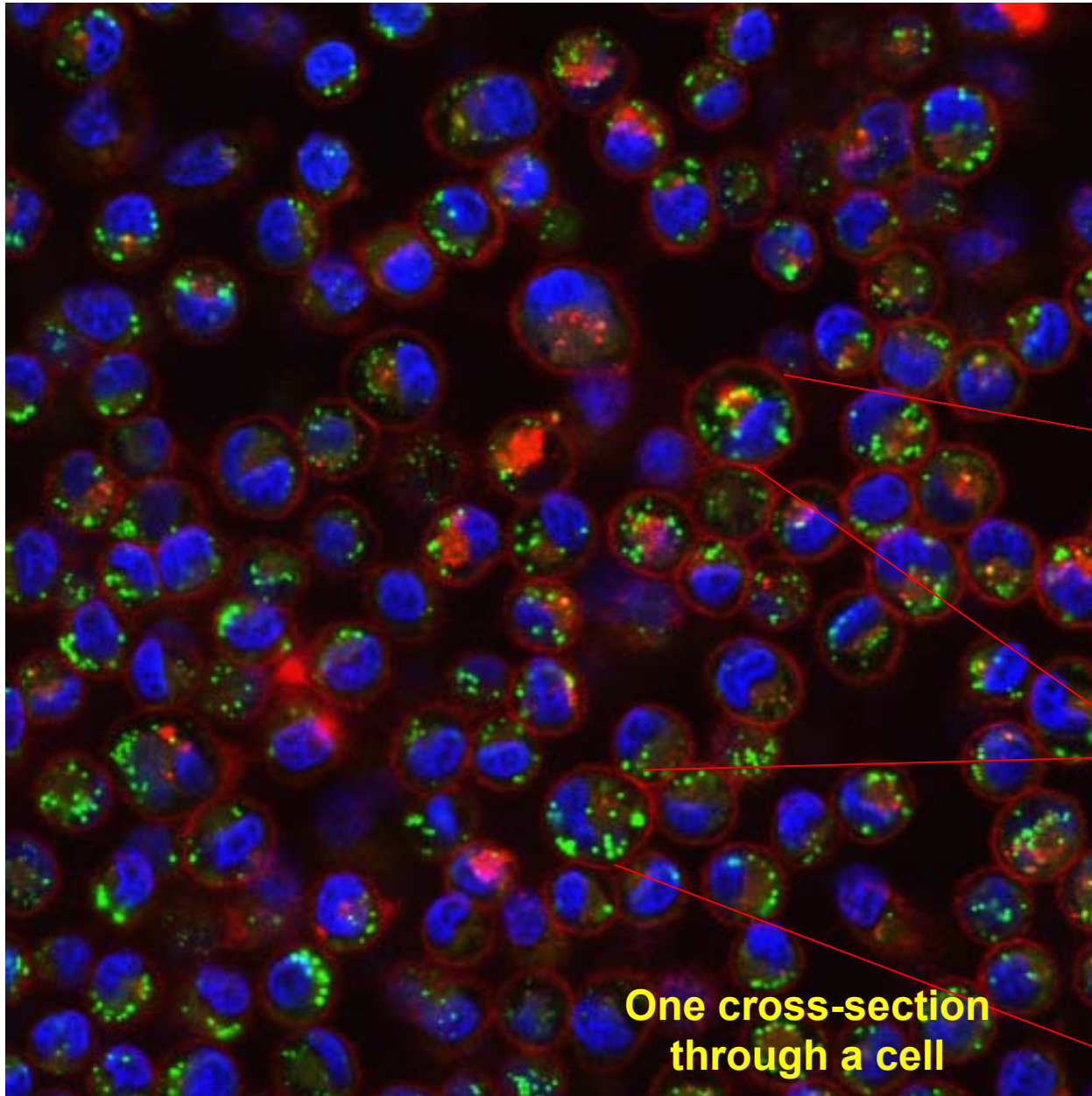
Q can increase by 100X by driving the cantilevers

Roukes, et. al.

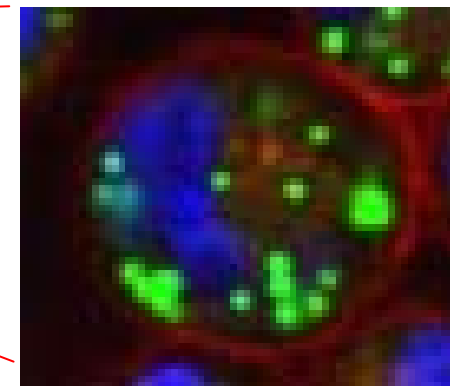
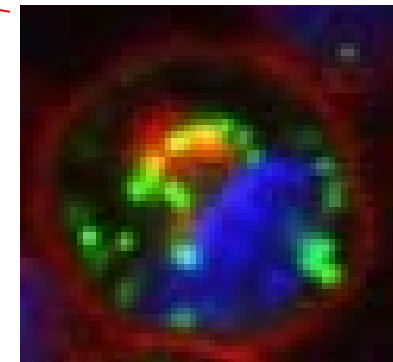


# 40nm NPs in KB Cancer Cells

- Bead incubation for 1 hour
- Particles are internalized by cells
- External beads rinsed and quenched by trypan blue dye



One cross-section  
through a cell

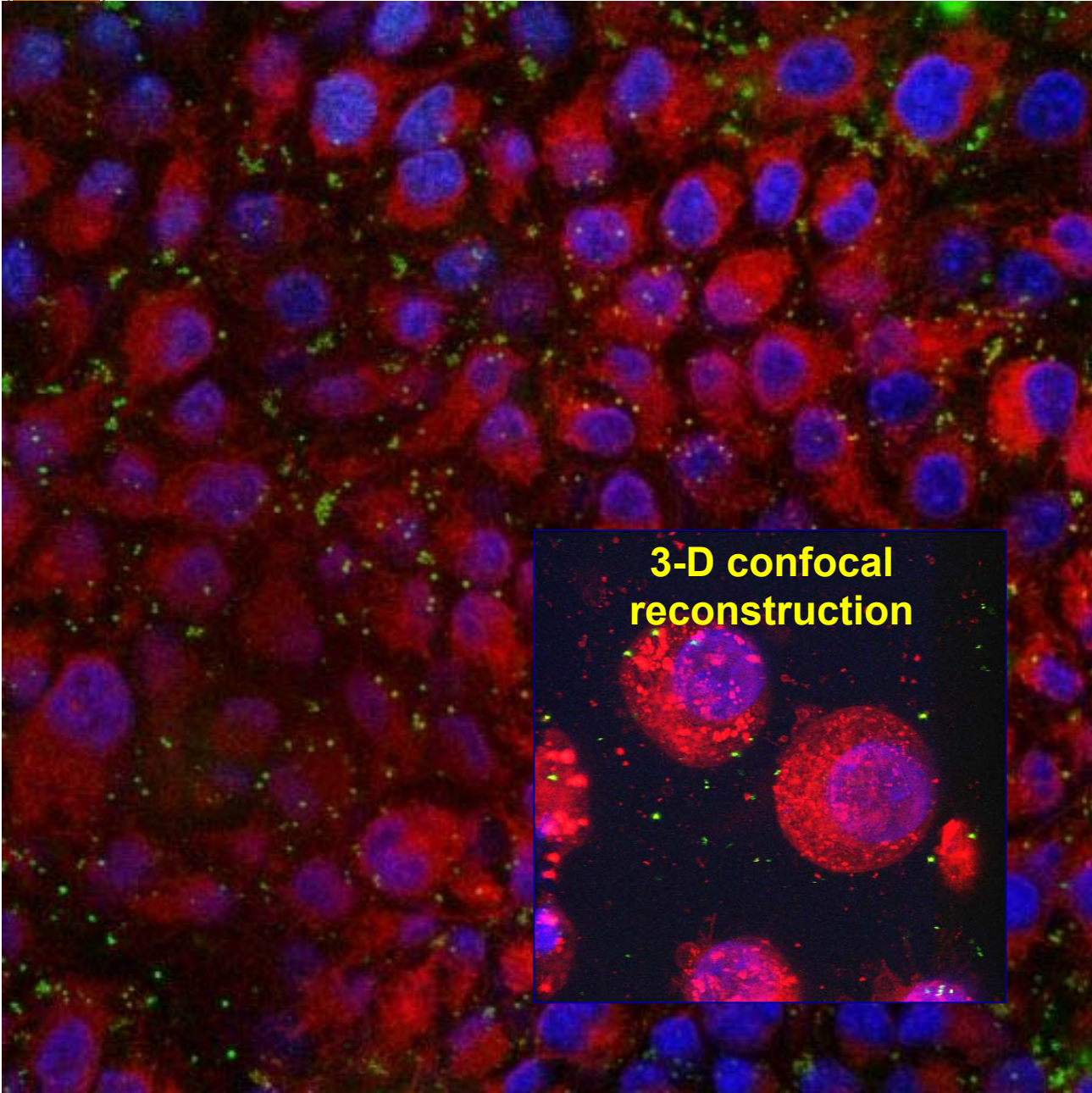






## 200nm Beads in KB Cells

- Bead incubation for 1 hour
- Confocal images – NPs are NOT internalized
- Cross-sectional scans



**3-D confocal  
reconstruction**



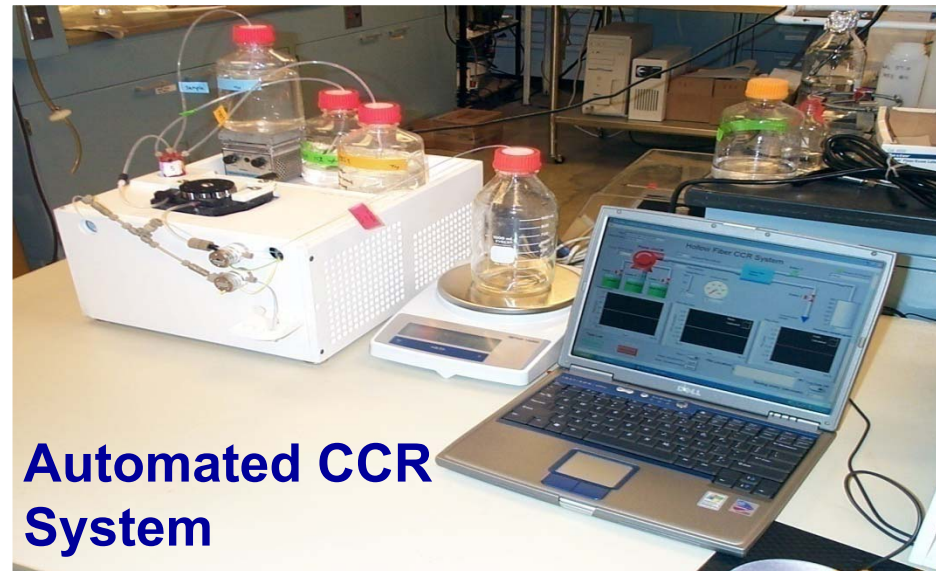
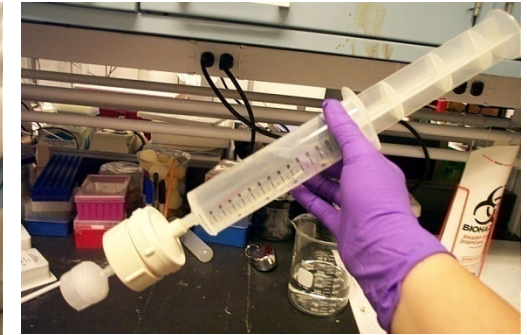
**One cross-section  
through one cell**





# Cell Concentration and Recovery

- Proprietary technology for cell concentration and recovery in small volumes – CCR™ kit
- One-time use filter cartridge
- Recovery rates ~ 50%



Chen, et al. *Biotech Bioengr*, 2005  
Huang, et al. *Submitted*, 2007

*Ladsich, et al. USDA Review, 2004*



# Recovery Results

## E. coli

100 ml sample in PBST

Run#	Initial cell conc. (cells/ml)	Final pressure drop (psi)	Recovery collection 1 (viable cells)	Total cells in collection 1	Recovery collection 2 (viable cells)	Recovery collection 3 (viable cells)	Leakage through permeate side	Total recovery (3 collections)
1	52±12	46	72.4±11.6%	3767±603	4.9±0.9%	0.4±0.1%	0.0±0.0%	77.7%
2	52±12	40	62.2±15.5%	3233±808	2.9±1.6%	0.5±0.3%	0.0±0.0%	65.5%
3	52±12	38	62.8±14.7%	3267±1531	4.0±1.1%	0.2±0.1%	0.0±0.0%	67.0%

## Listeria innocua

Run#	Initial cell conc. (cells/ml)	Final pressure drop (psi)	Recovery collection 1 (viable cells)	Total cells in collection 1	Recovery collection 2 (viable cells)	Recovery collection 3 (viable cells)	Leakage through permeate side	Total recovery (3 collections)
1	66±22	31	56.6±3.8%	3510±236	12.7±2.4%	0.9±0.4%	0.0±0.0%	70.2%
2	66±22	30	60.0±3.9%	3717±244	13.7±2.4%	2.3±0.7%	0.0±0.0%	75.9%
3	66±22	28	37.2±3.9%	2303±243	25.1±2.6%	6.0±0.6%	0.0±0.0%	68.2%

## Streptococcus faecalis

Run#	Initial cell conc. (cells/ml)	Final pressure drop (psi)	Recovery collection 1 (viable cells)	Total cells in collection 1	Recovery collection 2 (viable cells)	Recovery collection 3 (viable cells)	Leakage through permeate side	Total recovery (3 collections)
1	109±24	40	53.7±1.9%	5867±208	5.6±2.4%	1.7±0.3%	0.0±0.0%	61.0%
2	109±24	40	37.3±8.3%	4067±907	17.3±0.9%	2.4±0.3%	0.0±0.0%	56.9%
3	109±24	40	56.2±16.6%	6133±1815	6.4±0.3%	2.9±0.5%	0.0±0.0%	65.5%

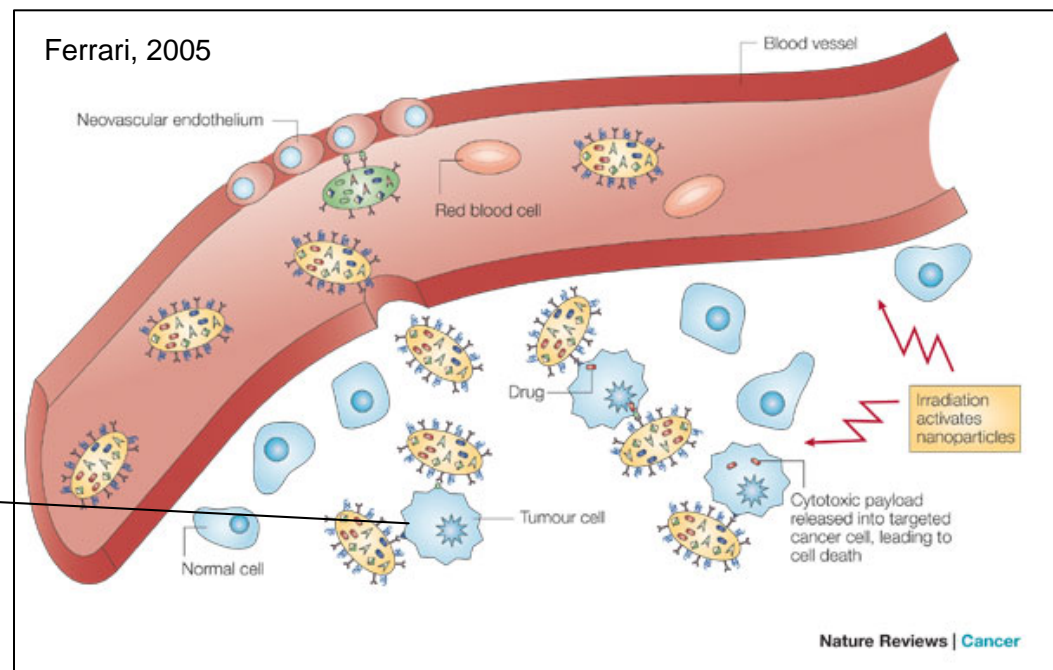
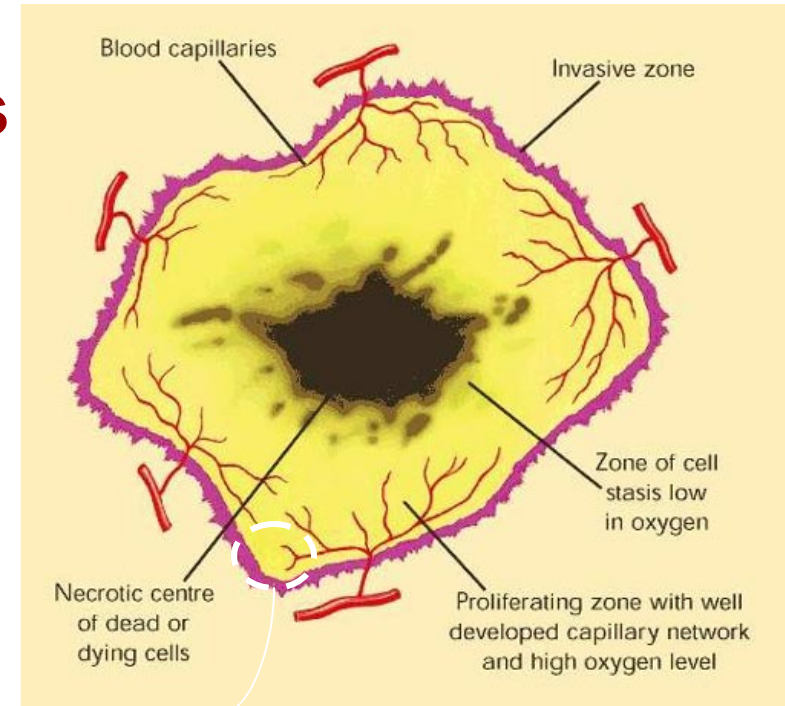
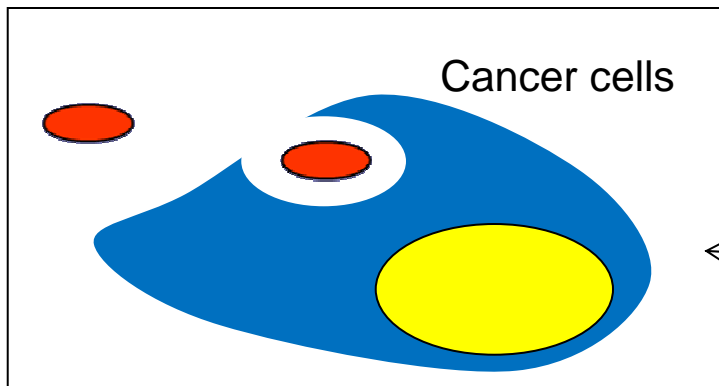


# Targeted Nano-therapeutics

## Objective:

To develop novel means to deliver nano-therapeutics to cancer cells and tumors

- Current drugs are ineffective at penetrating to the tumors due to inadequate vascularization at these tumor sites.
- Nanoparticles have the similar challenge of reaching tumor sites if adequate vascularization does not exist.
- Penetrate multiple barriers
- Need active transport to the cells and tumors





- Current drugs are ineffective at penetrating through the solid tumors due to inadequate vascularization at these tumor sites.
- Nanoparticles have the similar challenge of reaching tumor sites if adequate vascularization does not exist since they are carried by blood flow.

## **Bacterial Mediated Delivery of Nanoparticles in Cells**

**D. Akin, J.P. Robinson, S. Muhammad, A. Bhunia, R. Bashir**

### **Objective:**

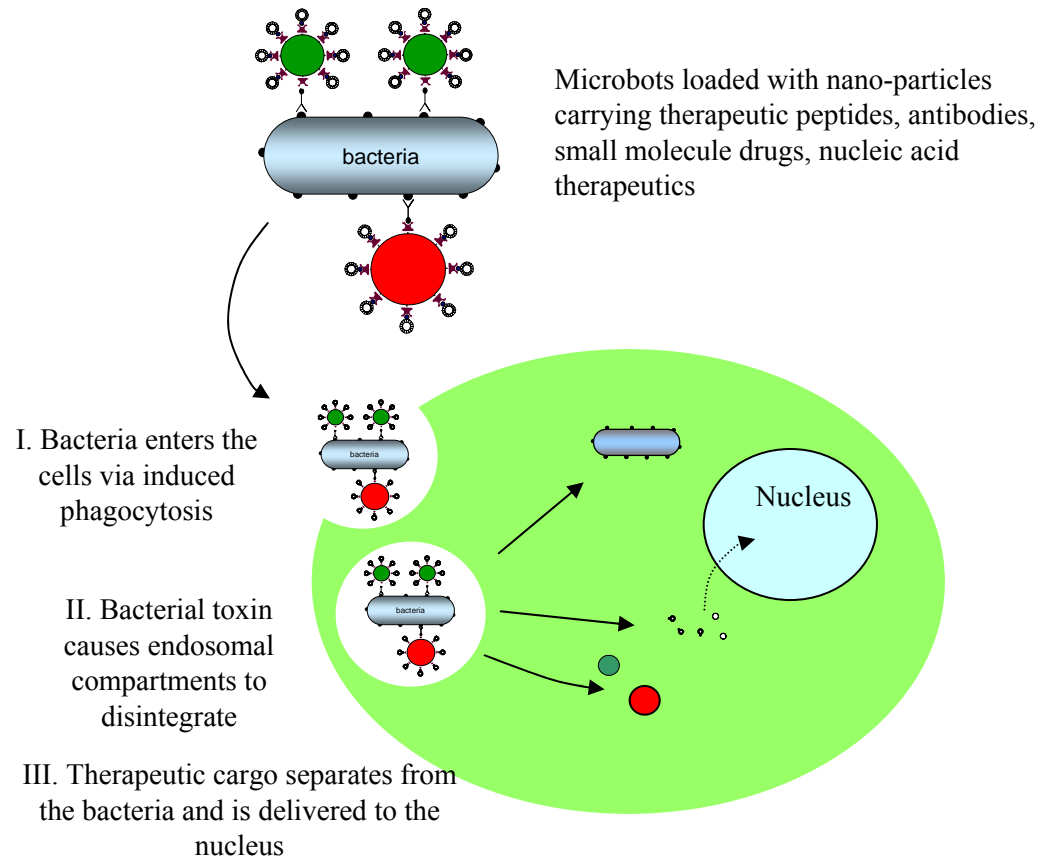
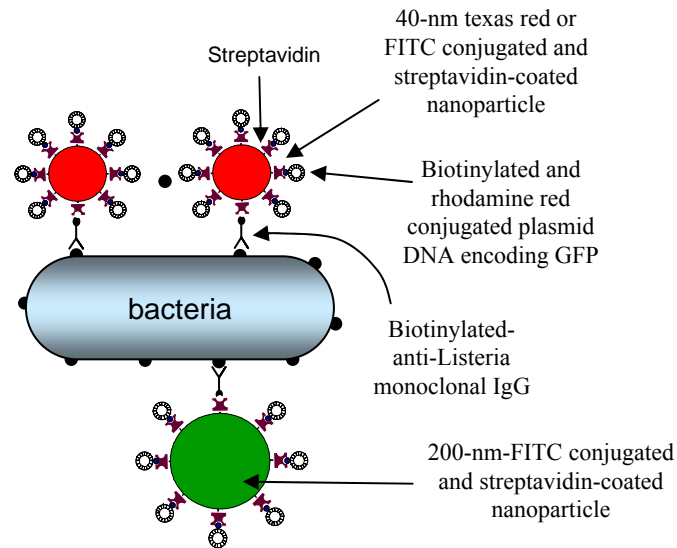
**To develop biologically-inspired intelligent devices for intracellular monitoring and therapeutic intervention of signal transduction networks**

### **Bacteria as a carrier !**

- Intracellular bacteria may provide means to penetrate and deliver therapeutic compounds to solid tumors that are otherwise inaccessible to drugs delivered by oral and parenteral routes.
- Bacteria can be engineered to have affinity for certain tumors.
- Bacteria can be engineered to express proteins on their surface for therapeutic or diagnostic intervention



# Functionalization Strategy

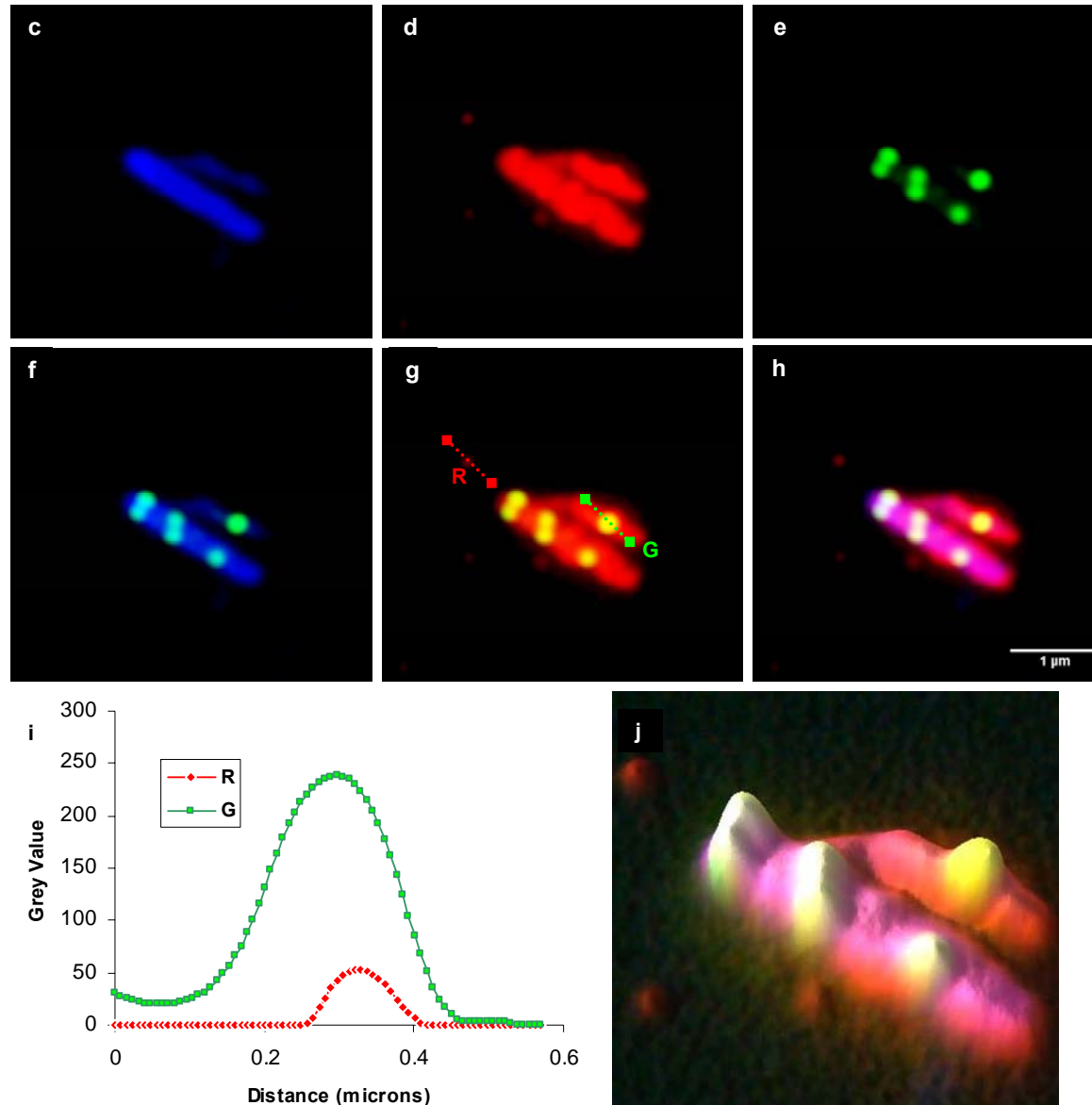


*D. Akin, J. Sturgis, K. Reghab, K. Burkholder, S. Muhammad, A. Bhunia, J. Robinson, R. Bashir, Nature Nanotechnology, 2007*



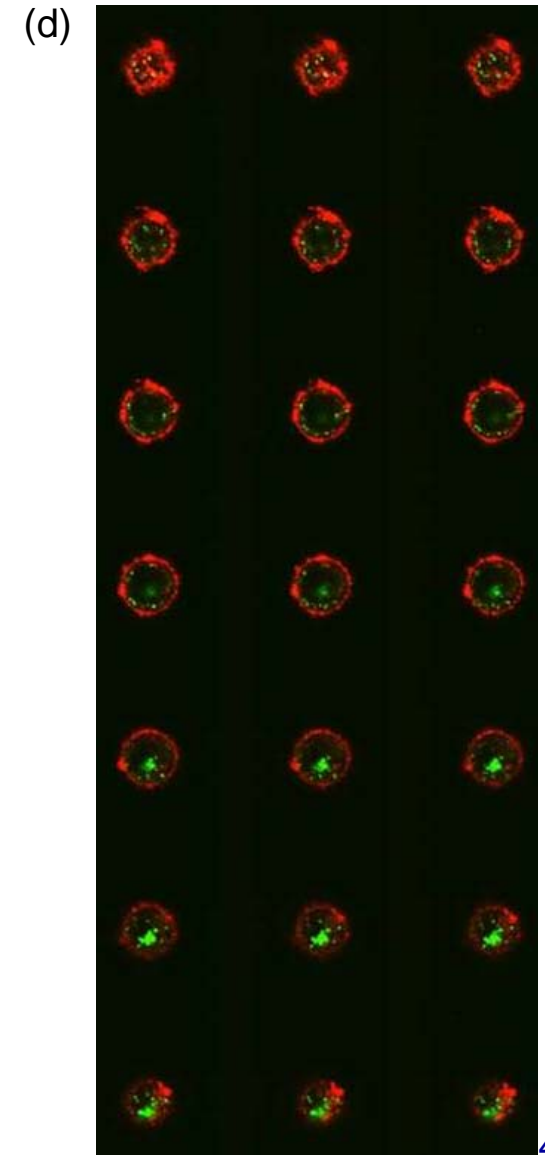
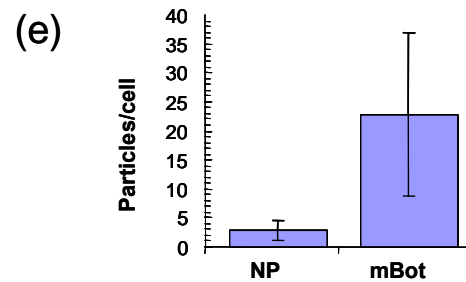
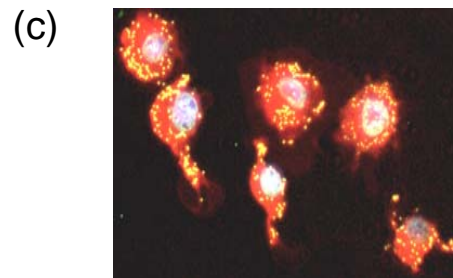
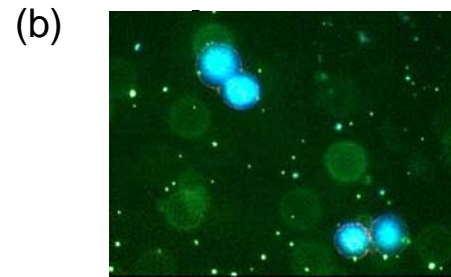
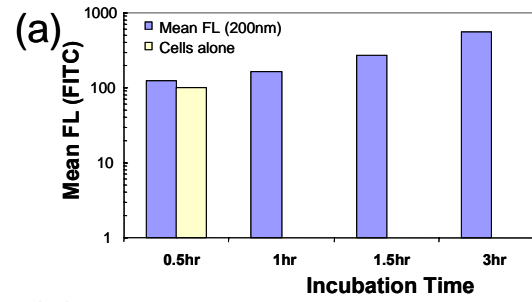
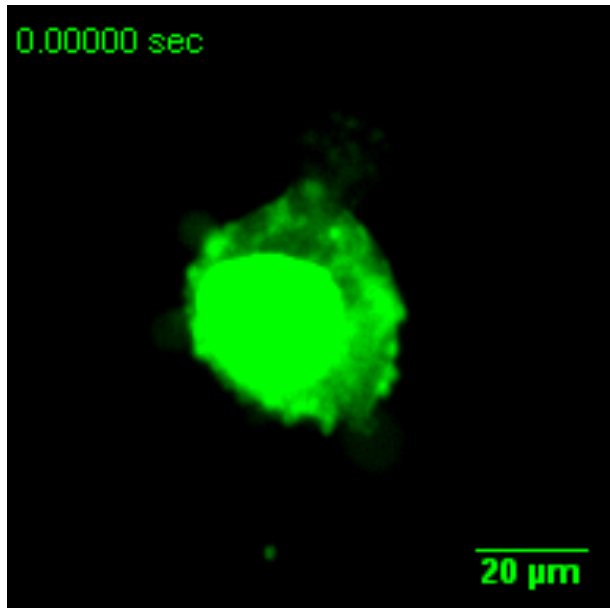
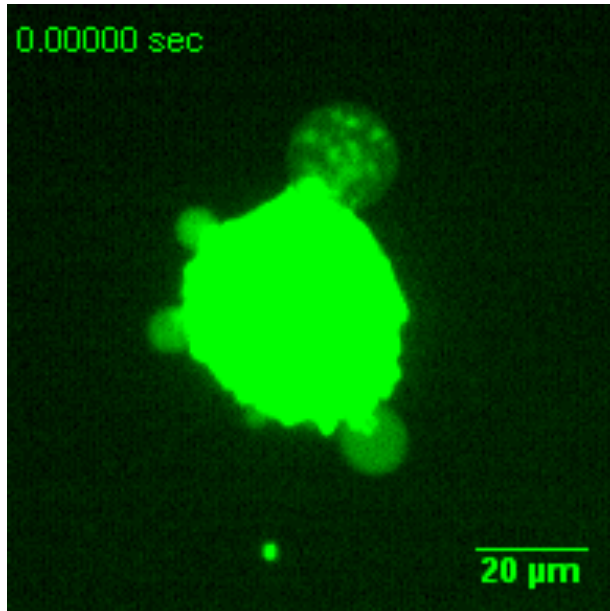


# Nanoparticles on Bacteria





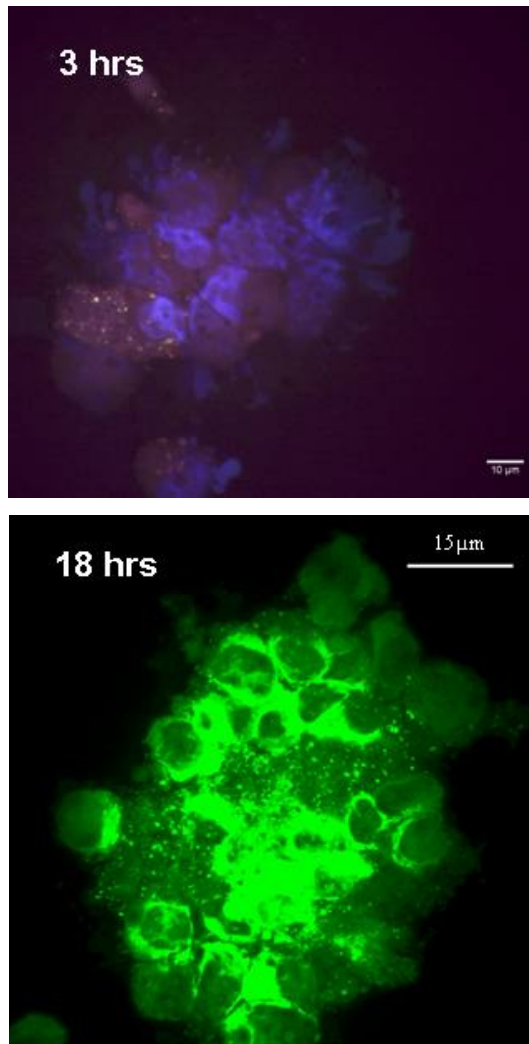
# Bacterial Mediated Delivery of NP



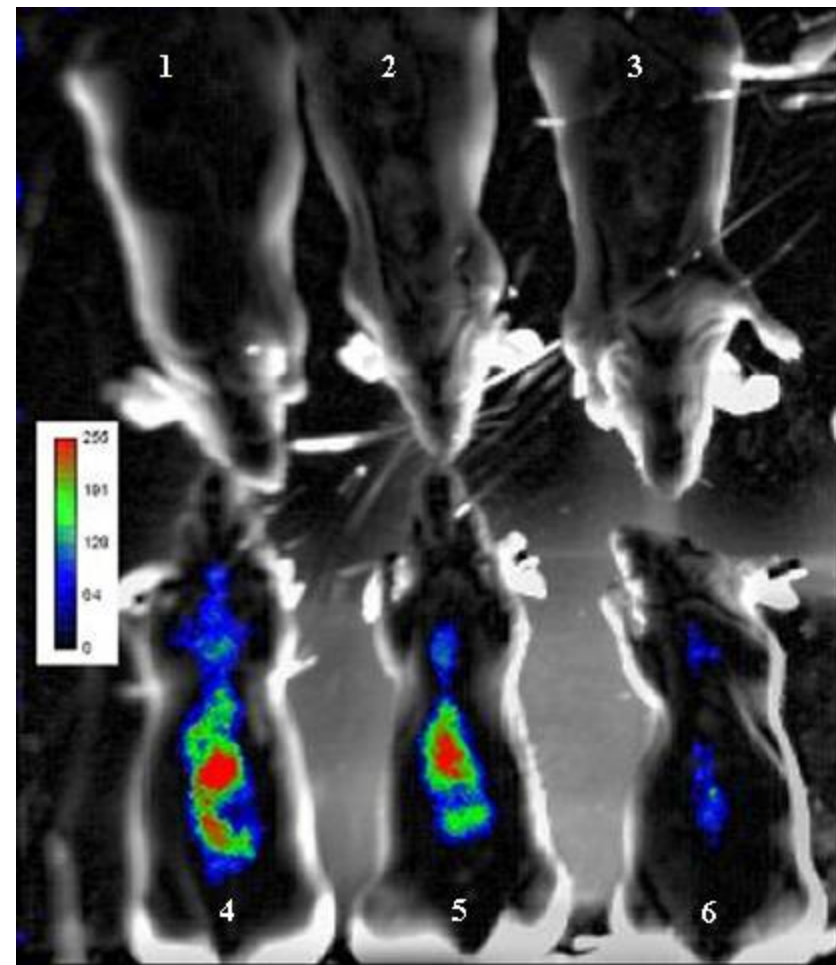


# Expression of GFP in KB Cells

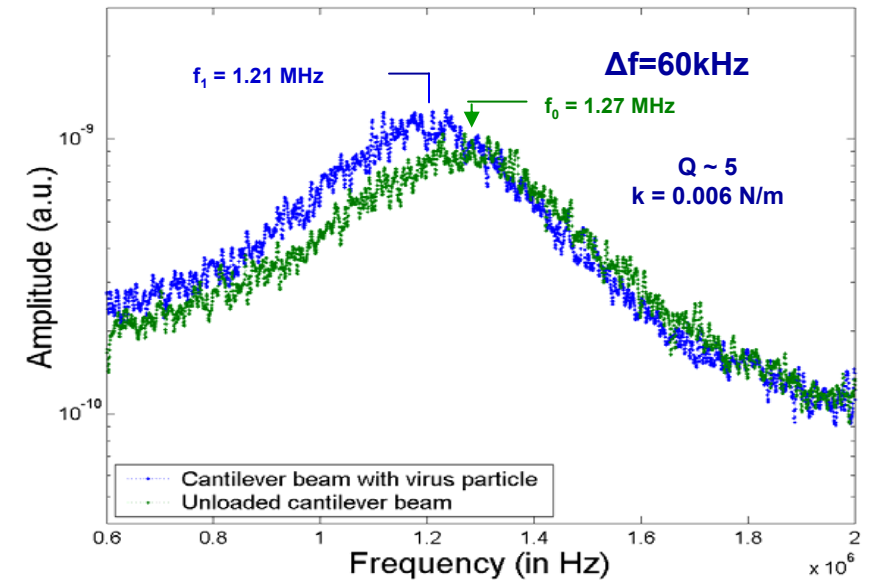
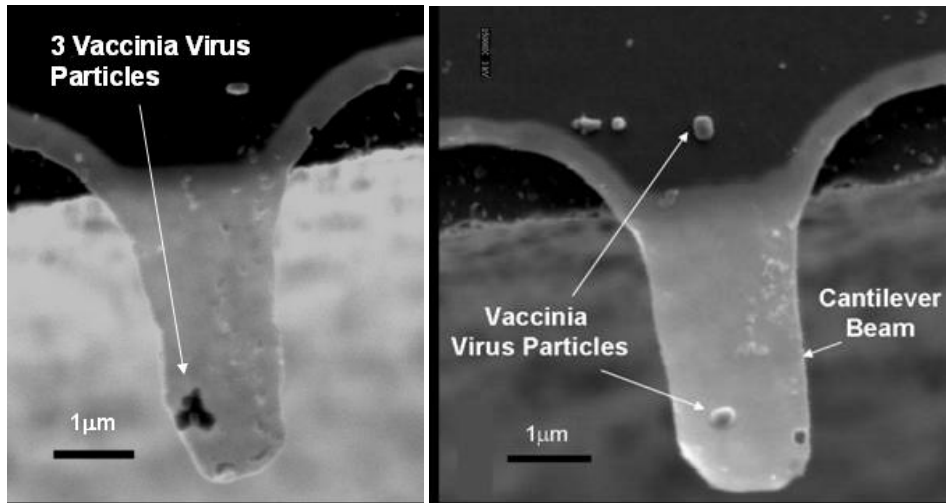
## Expression in-vitro in cells



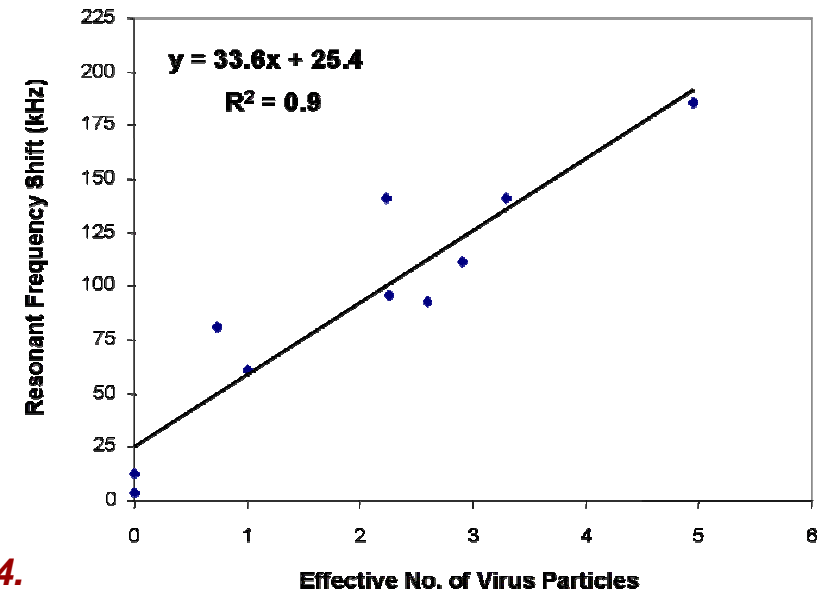
## Expression in-vitro in mice



*D. Akin, J. Sturgis, K. Reghab, K. Burkholder, S. Muhammad, A. Bhunia, J. Robinson, R. Bashir, Nature Nanotechnology, 2007*



**Work featured in Popular Science, EE Times, Nature News, and CNBC TV Show**



**A. Gupta, D. Akin, R. Bashir, Applied Physics Letters, 2004.**  
**A. Gupta, et al. Proc. Nat. Acad. Sci. 2006**